

## APPLICATION OF SYNTHETIC AND NATURAL POLYMERS IN PREPARATION AND CHARACTERIZATION OF DOMPERIDONE FAST-DISSOLVING FILMS

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## ABSTRACT

**Objective:** The present research work is mainly focused on solubility enhancement of domperidone which is a biopharmaceutical classification system Class II drug using natural and synthetic polymers.

**Methods:** The solubility was enhanced by the kneading method with the drug: polymer (1:0.5, 1:0.75, and 1:1) using  $\beta$ -cyclodextrin. The fast dissolving films (FDFs) of domperidone were prepared by incorporating the solid dispersion (SD) SDK3 by solvent casting method using hydroxypropyl methylcellulose K15 M (HPMC) and gellan gum in various concentrations for preparing FDFs. Various pre- and post-compression parameters, drug and excipients compatibility studies were evaluated by Fourier transform infrared (FTIR) spectroscopy, differential scanning calorimetry (DSC), and X-ray diffraction analysis (XRD).

**Results:** The maximum drug release of 98.86 % was achieved within 30 min for 1:1 ratio of solid dispersion using  $\beta$ -cyclodextrin, was optimized and taken for further development of FDFs. From the *in vitro* drug release studies films prepared with 10% w/w of HPMC K 15 (FH5) and 10% w/w of gellan gum (FG5) showed enhanced dissolution rate compared to other formulations. The formulation FHG with combination of polymers, namely, HPMC K 15 and gellan gum in 1:1 ratio showed drug release of 97.22% within 15 min only when compared with the optimized formulations. FTIR and DSC studies revealed that there were no interactions between drug and excipients. XRD studies revealed slight conversion of crystalline form to amorphous. The optimized formulation FHG found to be stable under accelerated stability studies.

**Conclusions:** The polymers in combination are a potential candidate for use in the formulation of FDF.

**Keywords:** Fast-dissolving film, Domperidone, Gellan gum, Hydroxypropyl methylcellulose,  $\beta$ -cyclodextrins, and Solid dispersion.

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## INTRODUCTION

Among the different routes of administration, the oral route of administration continues to be most preferred route due to various advantages including ease of administration, avoidance of pain, versatility, and most importantly patient compliance [1]. Many drugs given orally are poor in bioavailability because of the pH of the stomach, the presence of enzymes and extensive first-pass metabolism. Recent development in novel drug delivery system aims to enhance the safety and efficacy of drug molecules by formulating a convenient dosage form for administration [2,3]. Fast-dissolving oral delivery systems are solid dosage forms, which disintegrate or dissolve within 1 min when placed in the mouth without drinking water or chewing. The development of solid dosage films is given in Fig. 1 [4].

FDFs are the dosage forms which readily releases the drug by dissolving or when it comes in contact with the wet surface without the need of intake of water when compared with tablet due to increase in its surface area [5]. A film or strip can be defined as a dosage form that employs a water dissolving polymer (generally a hydrocolloid, which may be a bio adhesive polymer), which allows the dosage form to instantly wet by saliva [6]. The film quickly hydrates, adheres, then rapidly disintegrates and dissolves to release the medication for mucosal and intra gastric absorption when placed on the tongue or in the oral cavity to provide rapid local or systemic drug delivery [7,8]. This technology is also applicable for administration of low dose drugs and unpalatable drugs (domperidone, atenolol etc.) of Biopharmaceutical classification system (BCS) Class II drugs. In that case, for better release, the solubility of the drugs was improved by employing different solubility enhancement methods. One of the most commonly used techniques is solid dispersion (SD) which mainly includes different methods such as kneading method, neutralization method, solvent evaporation, and physical mixing [9-11]. Domperidone, a dopamine antagonist with an antiemetic and gastroprokinetic properties, is structurally related to the butyrophenones which do not cross the blood-brain barrier

and mainly act on the chemotrigger zone, located within the postrema zone [12]. The films are formulated using synthetic and hydrophilic polymers by employing kneading technique for solubility enhancement and solvent casting for the preparation of films [13].

## MATERIALS AND METHODS

## Materials

All materials used for the formulation were of analytical grade. Domperidone,  $\beta$ -cyclodextrin (CD), HPMC K4 M, HPMC K15 M, HPMC K100 M, gellan gum, glycerol citric acid, sodium starch glycolate, mannitol and Tween 80 were purchased from Yarrow Chem., Products, Mumbai. Ethanol from Changshu Yangyuan, China. Sodium hydroxide and potassium dihydrogen phosphate were purchased from Finar Limited, Ahmedabad.

## Method of preparation of SD

SDs were prepared with the different ratios of 1:0.5, 1:0.75 and 1:1 by kneading, physical and neutralization methods and evaluated for their drug content, percentage yield and dissolution properties in comparison with their respective physical mixtures [14-19].

## Preparation of domperidone FDFs using solvent casting method

The formulation of domperidone FDFs is given in Table 1. The films were prepared by dissolving film forming polymers and plasticizer as main constituents in water, later on addition of other remaining excipients with active pharmaceutical ingredient was added to the prepared solution. Different batches of formulations FH1-FH5 were formulated using HPMC grades, formulations FG1-FG5 were formulated using gellan gum as polymers and glycerol as a plasticizer by dissolving in an appropriate amount of water, formulation FHG was prepared by taking combination of HPMC and gellan gum and stirred for 4 h by maintaining 2000 rpm and kept aside for 1 h for the removal of entrapped air bubbles in the solution. Another solution was prepared by dissolving the other additives with Active pharmaceutical ingredient

Table 1: Composition of formulations

Ingredients (mg)	FH1	FH2	FH3	FH4	FH5	FG1	FG2	FG3	FG4	FG5	FHG
Ratio of API: CD	10	10	10	10	10	10	10	10	10	10	10
Hydroxypropyl methylcellulose K15	16	14	12	10	8	-	-	-	-	-	4
Gellan gum	-	-	-	-	-	16	14	12	10	8	4
Citric acid	4	4	4	4	4	4	4	4	4	4	4
Sodium starch glycolate	6	6	6	6	6	6	6	6	6	6	6
Mannitol	4	4	4	4	4	4	4	4	4	4	4
Tween 80	4	4	4	4	4	4	4	4	4	4	4
Total weight	44	42	40	38	36	44	42	40	38	36	36

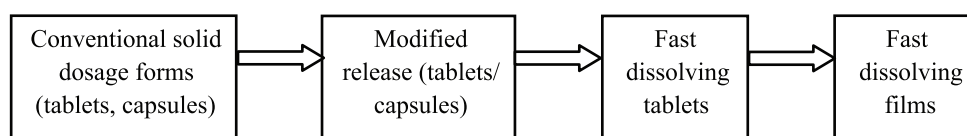


Fig. 1: Represents the development of solid dosage films

(API) in a hydro alcoholic solution and slowly added into the first solution and continued stirring for 1 h [20,21]. After completion of stirring, the solution was kept a side until the bubble free solution was obtained. Later, it was poured in Petri plate for obtaining the film and air-dried, as shown in Fig. 2.

Quantity sufficient of ethanol and water is taken for all formulations.

#### Characterization of prepared SD

The prepared SDs were evaluated for their drug content, percentage yield, and dissolution studies.

#### Determination of drug content

SD equivalent to 10 mg of domperidone was weighed accurately and was transferred to a 50 ml volumetric flask separately [1]. Volume was made up to 50 ml with methanol and subjected to sonication for dissolving domperidone. Appropriate dilutions were made with pH 6.8 phosphate buffer, and the amount of domperidone was observed in spectrophotometer (ElicoUV-1700 ultraviolet (UV)/visible double beam spectrophotometer) at 284 nm. The assay on each sample is replicated for 3 times. The drug content was calculated using Equation 1.

$$\% \text{Drug content} = \frac{\text{Actual drug content}}{\text{Theoretical drug content}} \times 100 \quad (1)$$

#### Determination of percent yield

The percent yield of prepared SDs was determined by utilizing the formula given in Equation 2 using the total recoverable final weight of SD and the total original weights of drug and carriers used [22].

$$\text{Percent yield} = \left[ \frac{a}{(b-c)} \right] \times 100 \quad (2)$$

#### In vitro dissolution studies

The drug release from the prepared SD was studied using eight station dissolution rate test apparatus (Lab India, Disso 2000) employing a paddle stirrer at 75 rpm and at  $37 \pm 0.5^\circ\text{C}$ . Phosphate buffer of pH 6.8 (900 ml) was used as dissolution fluid. At predetermined intervals, the aliquots sample was withdrawn and replaced with fresh media. The absorbance of these solutions was measured at 284 nm using spectrophotometer. The same process was used for domperidone FDFs.

#### Evaluation of domperidone FDFs

All the prepared domperidone FDFs were evaluated for thickness, dry test/tack test, tensile strength, percent elongation, tear resistance, Young's modulus, folding endurance, swelling properties, transparency, content uniformity, disintegration time, and *in vitro* dissolution test [23-25].

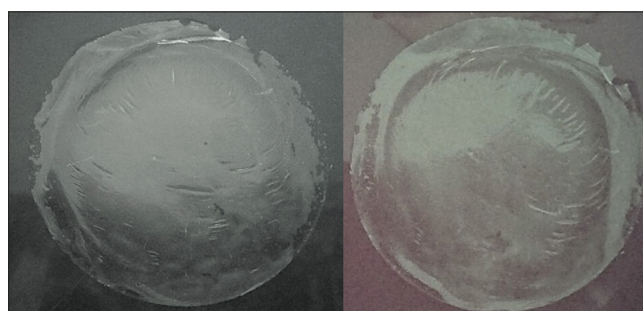


Fig. 2: Prepared domperidone FDFs

#### Thickness

The thickness of the strip can be measured by Vernier calipers at different strategic locations. This is essential to ascertain uniformity in the thickness of the film as this is directly related to the accuracy of dose in the strip.

#### Percent elongation

When stress is applied, a strip sample stretches, and this is referred to as strain. Strain is basically the deformation of strip divided by original dimension of the sample, as given in Equation 3. In general, elongation of strip increases as the plasticizer content increases.

$$\% \text{Elongation} = \frac{\text{Increase in length of strip}}{\text{Initial length of strip}} \times 100 \quad (3)$$

#### Folding endurance

Folding endurance is determined by repeated folding of the strip at the same place until the strip breaks. The number of times the film is folded without breaking is computed as the folding endurance value.

#### Swelling property

Film sample is weighed and placed in a pre-weighed stainless-steel wire mesh. The mesh containing a film sample is submerged into 15 ml medium in a plastic container. The weight of the film was measured after the preset time interval after attaining of constant weight. The degree of swelling is calculated using formula:

$$\alpha = \frac{W_t - W_o}{W_o} \quad (4)$$

Where:  $W_t$  is weight of film at time  $t$  and  $W_o$  is weight of film at time zero.

**Transparency**

The film samples were cut into rectangles and placed on the internal side of the UV spectrophotometer cell and the transmittance of films was analyzed at 600 nm. The transparency of the films can be calculated as follows:

$$\text{Transparency} = \frac{\log T_{600}}{b} = -\epsilon c \quad (5)$$

Where:  $T_{600}$  is the transmittance at 600 nm,  $b$  is the film thickness (mm), and  $c$  is concentration.

**Table 2: Percent drug content and percent yield of prepared solid dispersions**

Drug: Beta cyclodextrins mass ratio	Formulation code	Drug content (%)*	Percent yield*
1:0.5	SDK1	89.34±0.25	83.77±0.52
1:0.75	SDK2	93.48±0.32	85.97±0.38
1:1	SDK3	96.86±0.08	94.5±0.32

\*Mean percent of domperidone released and obtained (mean±SD (n=3))

**Table 3: Correlation coefficient analysis of formulations**

Formulation code	Correlation coefficient (r-value)			
	Zero-order model	First-order model	Higuchi model	Erosion plot
PD	0.9014	0.9525	0.9859	0.9375
SDK1	0.9009	0.9533	0.9905	0.9381
SDK2	0.7132	0.8353	0.8805	0.7921
SDK3	0.6893	0.9472	0.8734	0.8539

**Table 4: Drug release characteristics of the prepared solid dispersions**

Formulation code	Polymer concentration (%)	$T_{50}$ (min)	$T_{90}$ (min)	$K_0$ (mg/h)	$K_1/h$	'n' in Peppas equation
PD	-	30	>60	0.9786	0.0067	0.5952
SDK1	1:0.5	12.5	>60	0.9547	0.0066	0.5169
SDK2	1:0.75	9.5	43	1.4114	0.0171	0.5566
SDK3	1:1	7.5	15	1.5129	0.0370	0.4968

**Table 5: Film properties of formulations**

Evaluation parameters	FH1	FH2	FH3	FH4	FH5
%Drug content <sup>a</sup>	97.51±0.89	98.04±0.74	98.32±1.18	97.89±0.46	98.69±0.98
Thickness <sup>b</sup>	0.23±0.08	0.21±0.15	0.23±0.12	0.23±0.18	0.22±0.09
Weight variation <sup>b</sup>	58.45±0.08	59.18±0.96	58.33±0.54	57.67±0.43	57.89±0.88
Surface pH <sup>a</sup>	6.92±0.13	6.78±0.11	6.96±0.14	6.84±0.12	6.25±0.16
Folding endurance <sup>a</sup>	256±1.13	242±0.52	338±0.32	286±0.67	318±0.34
Swelling property <sup>a</sup>	0.42±0.14	0.64±0.04	0.45±0.06	0.78±0.05	0.76±0.08
Transparency <sup>a</sup>	Transparent	Transparent	Transparent	Transparent	Transparent
Disintegration time <sup>a</sup>	35.0±0.5	29.0±0.49	32.0±0.35	28.0±0.78	27.0±0.34
% Elongation <sup>a</sup>	69.27±0.87	54.65±0.32	52.65±0.78	32.67±0.34	24.56±0.96

Where: <sup>a</sup>mean±s.d.(n=3) of domperidone FDFs, <sup>b</sup>mean±s.d. (n=10) of domperidone FDFs

**Table 6: Film properties of formulations**

Evaluation parameters	FG1	FG2	FG3	FG4	FG5	FHG
%Drug Content <sup>a</sup>	98.2±1.11	98.4±0.78	97.8±0.68	98.9±0.46	98.6±0.32	98.9±0.88
Thickness <sup>b</sup>	0.21±0.08	0.22±0.01	0.22±0.07	0.23±0.06	0.22±0.11	0.22±0.05
Weight variation <sup>b</sup>	58.2±0.42	58.7±1.05	58.8±0.95	58.2±0.89	57.9±0.76	58.3±0.52
Surface pH <sup>a</sup>	6.52±0.12	6.76±0.08	6.63±0.11	6.70±0.05	6.90±0.10	6.43±0.04
Folding Endurance <sup>a</sup>	302±0.92	295±0.54	287±0.67	312±0.83	298±0.32	308±0.53
Swelling property <sup>a</sup>	0.49±0.03	0.68±0.05	0.75±0.05	0.59±0.02	0.84±0.04	0.86±0.06
Transparency <sup>a</sup>	Transparent	Transparent	Transparent	Transparent	Transparent	Transparent
Disintegration time <sup>a</sup>	34±0.47	27±0.63	28±0.53	29±0.63	26±0.38	27±0.45
% Elongation <sup>a</sup>	59.8±0.56	69.8±0.85	64.7±0.43	51.8±0.60	25.7±0.64	28.93±0.49

Where: <sup>a</sup>mean±s.d. (n=3) of domperidone FDFs, <sup>b</sup>mean±s.d. (n=10) of domperidone FDFs

**Content uniformity**

Content uniformity was determined by estimating the domperidone content in an individual strip using pH 6.8 phosphate buffer suitably diluted and the amount of drug present was estimated at 284 nm using UV spectrophotometer.

**Disintegration time**

The formulated films were subjected to the disintegration test using standard apparatus as mentioned in the reference pharmacopeias using pH 6.8 phosphate buffer.

**Drug excipient compatibility studies***Visual inspection*

The compatibility of the drug and excipients was observed by visual inspection by placing the appropriate amount of the drug alone or in combination with other excipients in glass vials for about 3 months.

*Fourier transform infrared (FTIR) spectroscopy*

The interaction between drugs and excipients was investigated with the help of FTIR spectrophotometer (Shimadzu, Japan, FTIR-8400S). Test samples were placed in the side KBr discs (with a ratio of 1:100 of test sample within KBr was maintained) and compressed at applied hydrostatic pressure of 5.2 N/m<sup>2</sup> for about 180 s. The range of scanning was between 400 and 4000 cm<sup>-1</sup>.

*Differential scanning calorimetry (DSC)*

DSC is generally used to investigate and predict any physicochemical interactions between components in the formulation and therefore can be applied to the selection of suitable chemically compatible excipients. The DSC analysis of pure drug and the excipients was carried out to evaluate any possible drug-polymer interactions. The analysis was

performed at a rate of 40°C/min conducted over a temperature range of 40–300°C.

#### X-Ray diffraction analysis (XRD)

XRD analysis is an important tool investigation tool for evaluating the crystal structure as well as the average structural spacing between the layers and rows of atoms in an unknown material. Both for pure drug and the drug-loaded films, XRD studies were performed utilizing an XRD (Rigaku, Japan). A 400 kV, 30 mA Cu-K $\alpha$  radiations were maintained at a scanning speed of 10/min to identify the physical state of drug as well as drug-loaded films.

#### Data analysis

Release data were analyzed as per zero-order, first-order, Higuchi, and Peppas equation models to assess the drug release kinetics and mechanism from the matrix tablets prepared [26,27].

#### Stability studies

The optimized formulations were accurately weighed, the amount of sample was placed in glass vials and stored for 1–3 months and

evaluated for physical parameters, drug content and drug release studies.

## RESULTS AND DISCUSSION

All the prepared SDs by kneading method showed free-flowing. The values of % drug content and % yield are given in Table 2 and were found to be in the range of 89.34–96.86% and 83.77–94.5%, respectively. The drug content analysis indicated that domperidone was uniformly distributed in the SDs prepared by kneading method.

The *in vitro* dissolution profiles, as shown in Fig. 3, have shown distinct deviation in the plots, when the concentration of polymer is increased the %drug release was increased from 85.73, 89.48, and 99.29%.

The correlation coefficient (r) values in the analysis of the release data are given in Table 3. The release data indicated that the domperidone release from the SDs followed first-order kinetics with diffusion controlled. When the release data were analyzed as per Peppas equation, the release exponent “n” was in the range 0.51–0.59 indicating non-Fickian (anomalous) diffusion as the release mechanism and values are given in Table 4. From the results, formulation SDK3 is optimized.

#### Evaluation of domperidone FDFs

The prepared domperidone FDFs were evaluated for thickness, percent elongation, folding endurance, swelling property, transparency, %drug content, weight variation, surface pH, disintegration time and *in vitro* dissolution studies. The results are shown in Tables 5 and 6.

#### *In vitro* dissolution studies of FDFs

All the formulations were evaluated for *in vitro* dissolution. As the concentration of the polymers, HPMC K15M and gellan gum increased the swelling of the film, disintegration time increased and %drug release retarded. At lower concentration, the disintegration time decreased and %drug release increased within 20 min. Hence, formulation with lower concentration of polymer was optimized and adopted in the preparation of FDFs to achieve the aim of the present research work. The drug release profiles are shown in Fig. 4. The drug release data were analyzed as per zero-order, first-order, Higuchi, Erosion, and Peppa's equation models. The correlation coefficient (r) values in the analysis of the release data as

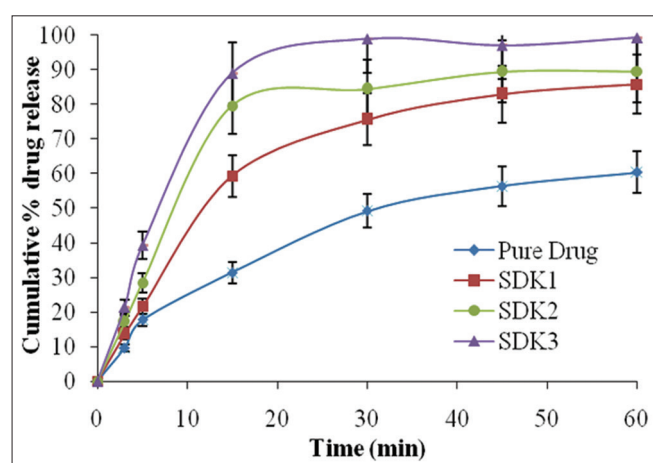


Fig. 3: Dissolution profiles of SD formulations

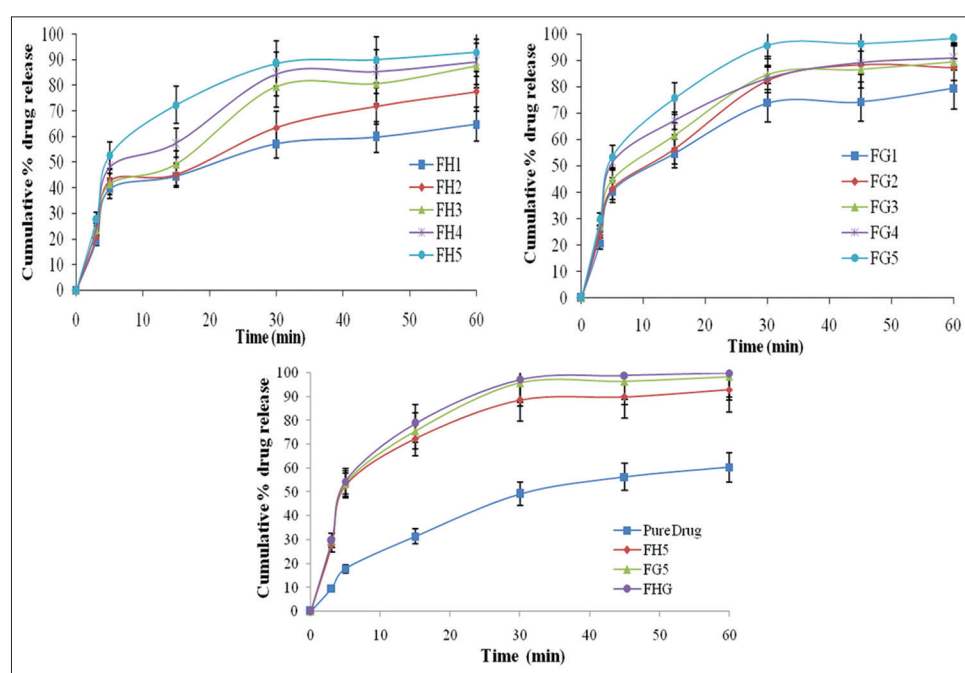


Fig. 4: Dissolution profiles of FDFs formulations



Table 7: Correlation coefficient analysis of formulations

Formulation code	Correlation coefficient (r-value)			
	Zero-order model	First-order model	Higuchi model	Erosion plot
FH 1	0.7167	0.8301	0.8974	0.7941
FH 2	0.7980	0.9301	0.9387	0.8928
FH 3	0.8128	0.9393	0.9522	0.9071
FH 4	0.7570	0.9089	0.9245	0.8686
FH 5	0.6950	0.9027	0.8927	0.8424

Table 8: Correlation coefficient analysis of formulations

Formulation code	Correlation coefficient (r-value)			
	Zero-order model	First-order model	Higuchi model	Erosion plot
FG 1	0.7577	0.8828	0.9288	0.8462
FG 2	0.7888	0.9063	0.9460	0.8785
FG 3	0.7586	0.9149	0.9336	0.8728
FG 4	0.7252	0.9291	0.9111	0.8718
FG 5	0.7072	0.9499	0.9018	0.8861
FHG	0.6986	0.9912	0.8959	0.9202

per different kinetic models are given in Tables 7 and 8. All the prepared formulation FH1-FH5, FG1-FG5, and FHG followed first-order kinetics. According to Korsmeyer-Peppas equation, the release exponent "n" value was used to characterize different release mechanisms. If the n value is 0.45, the release mechanism follows Fickian diffusion. If n value is  $0.45 < n < 0.89$  (for cylindrical), the mechanism follows non-Fickian (anomalous) diffusion, and when n value is 0.89 it will be non-Fickian case II transport, and if  $n > 0.89$  it will be non-Fickian super case II transport. The drug release characteristics of the prepared domperidone FDFs are given in Tables 9 and 10. All the formulations followed non-Fickian (anomalous) diffusion mechanism.

#### Compatibility studies of FDFs

##### Visual inspection

Visual inspection was conducted to check the compatibility between drug and excipients in the film when stored in a glass container at room temperature for 3 months. Throughout the examination, there was no change in the color of the film, indicating that drug and excipients are quite compatible.

##### FTIR spectroscopy

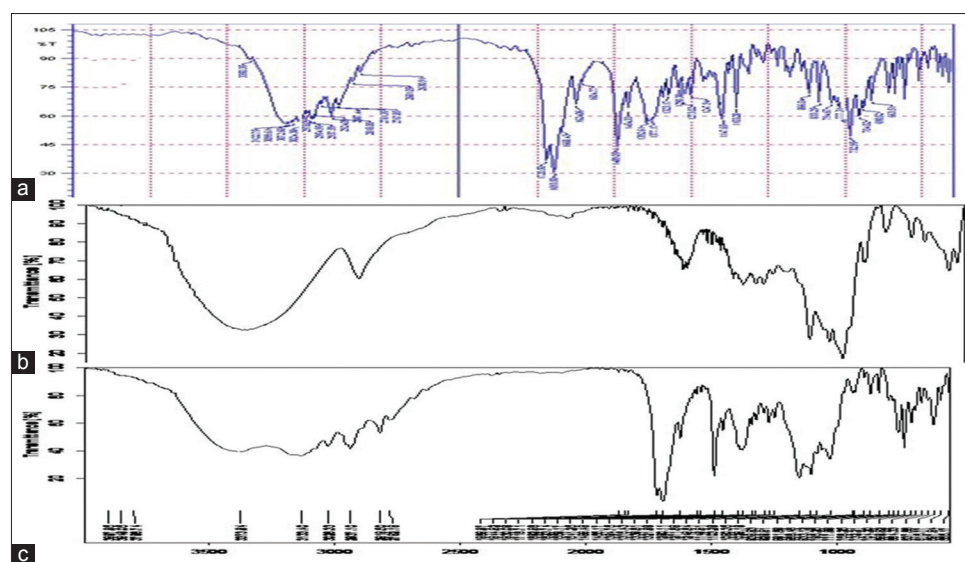
Domperidone,  $\beta$ -cyclodextrin and optimized SD were characterized by FTIR spectrum by KBr disc method and are shown in Fig. 5. The

Table 9: Drug release characteristics of formulations

Formulation code	Polymer concentration (%)	T <sub>50</sub> (min)	T <sub>80</sub> (min)	K <sub>0</sub> (mg/h)	K <sub>1</sub> /h	'n' in Peppas equation
FH 1	20	20	>60	0.8641	0.0065	0.3375
FH 2	17.5	19.5	>60	1.0815	0.0098	0.3727
FH 3	15	15	30	1.2798	0.0144	0.4066
FH 4	12.5	5.5	28	1.2799	0.0157	0.3885
FH 5	10	4.25	22	1.2841	0.0185	0.3609

Table 10: Drug release characteristics of formulations

Formulation code	Polymer concentration (%)	T <sub>50</sub> (min)	T <sub>80</sub> (min)	K <sub>0</sub> (mg/h)	K <sub>1</sub> /h	'n' in Peppas equation
FG 1	20	10	>60	1.1382	0.0108	0.4059
FG 2	17.5	9.5	35	1.3175	0.0158	0.4178
FG 3	15	12.5	32	1.2843	0.0161	0.3788
FG 4	12.5	5	26	1.2723	0.0170	0.3673
FG 5	10	4.25	18	1.3868	0.0297	0.3693
FHG	5+5	4	12.5	1.4111	0.0439	0.3737

Fig. 5: FTIR spectra of (a) Domperidone (b)  $\beta$ -cyclodextrin and (c) SDK3

FTIR spectrum of pure domperidone [20,28,29] showed characteristic N-H stretch at  $3364.91\text{ cm}^{-1}$  and strong C=O stretch at  $1694.45\text{ cm}^{-1}$ , indicating the presence of -CONH group, asymmetric =C-H stretching at  $3072.20\text{ cm}^{-1}$ , symmetric -C-H stretching at  $2955.19\text{ cm}^{-1}$ , aromatic C-H stretching at  $3024.18\text{ cm}^{-1}$ , -C=C- stretch at  $1622.48\text{ cm}^{-1}$ , and C-Cl stretch denoting the presence of alkyl halide at  $731.50\text{ cm}^{-1}$ .

The FTIR spectrum of  $\beta$ -cyclodextrin showed characteristic N-H stretch at  $3382.52\text{ cm}^{-1}$  and strong C=O stretch at  $1636.50\text{ cm}^{-1}$ , indicating the presence of -CONH group, asymmetric =C-H stretching at  $2924.32\text{ cm}^{-1}$ , symmetric -C-H stretching at  $2955.19\text{ cm}^{-1}$ , aromatic C-H stretching at  $3044.18\text{ cm}^{-1}$ , -C=C- stretch at  $1749.46\text{ cm}^{-1}$ , and C-Cl stretch denoting the presence of alkyl halide at  $947.12$  and  $757.46\text{ cm}^{-1}$ .

The spectra of SD showed similar characteristic stretches present in the pure drug such as N-H stretch at  $3373.92\text{ cm}^{-1}$  and

asymmetric =C-H stretching at  $3026.33\text{ cm}^{-1}$ , symmetric -C-H stretching at  $2937.10\text{ cm}^{-1}$ , -C=C- stretch at  $1559.17\text{ cm}^{-1}$ , and C-Cl stretch denoting the presence of alkyl halide at  $756.26\text{ cm}^{-1}$ . However, the spectrum did not show any additional peak indicating the absence of any chemical reaction between the domperidone and  $\beta$ -cyclodextrin [14,15].

#### DSC

DSC thermograms of domperidone,  $\beta$ -cyclodextrin, HPMC K15M, gellan gum, optimized SD and FDFs are shown in Fig. 6 corresponding to the melting point of the pure drug in its official monograph as per USP. The melting endothermic peak of domperidone in its pure form was observed at  $245.98^\circ\text{C}$  with onset at  $250.3^\circ\text{C}$  and  $\Delta H$  of  $6.42\text{ mJ/mg}$ .  $\beta$ -cyclodextrin showed a sharp endothermic peak at  $91.27^\circ\text{C}$  with enthalpy of fusion ( $\Delta H$ ) of  $161.10\text{ mJ/mg}$  corresponding with the  $\beta$ -cyclodextrin melting temperature.

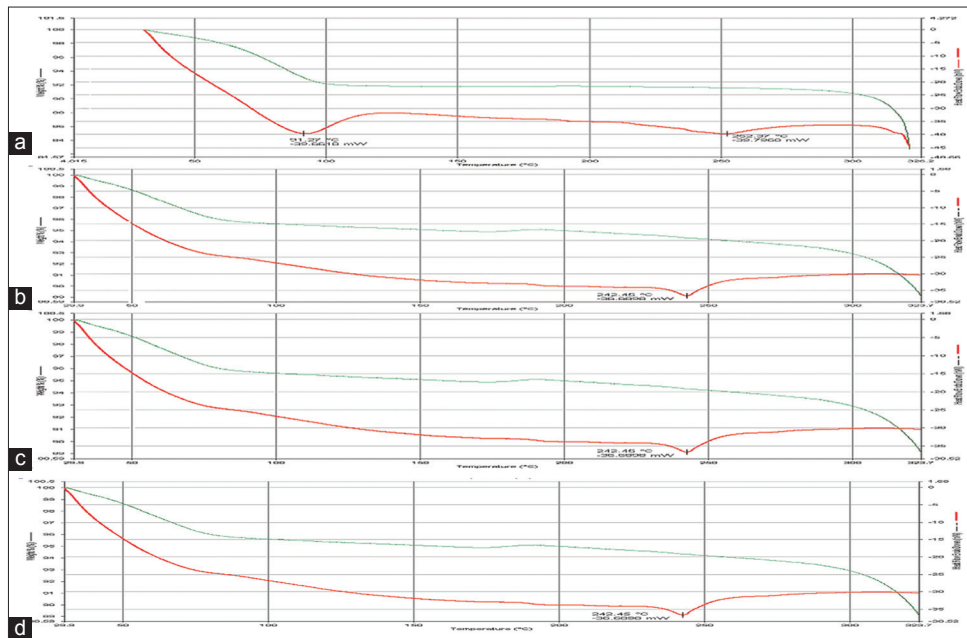


Fig. 6: Differential scanning calorimetry thermograms of (a) Domperidone, (b)  $\beta$ -cyclodextrin, and (c) SDK3, and (d) FDF FHG

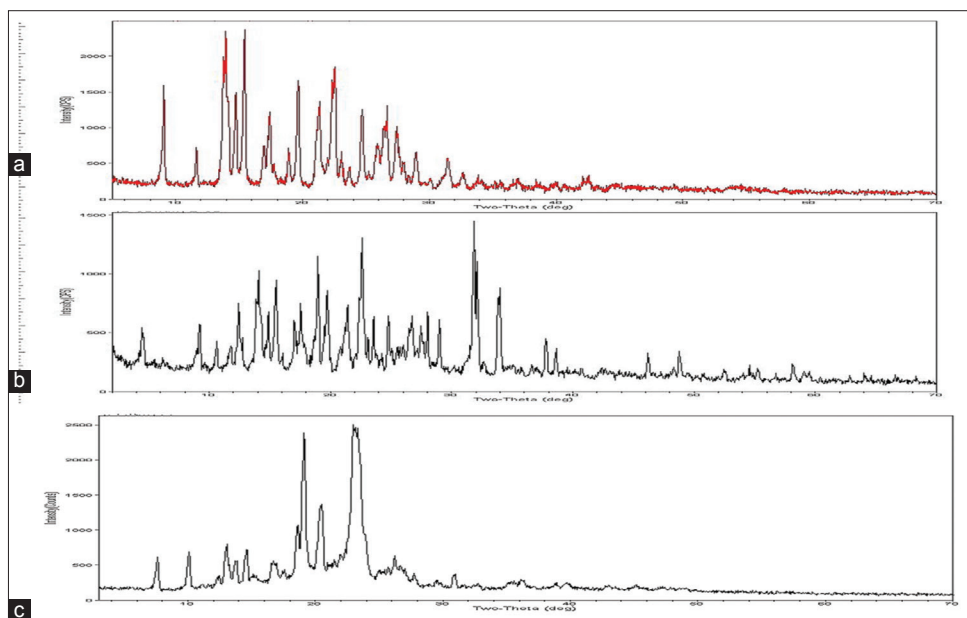


Fig. 7: Dissolution profiles of optimized formulation FHG on stability

From the curves of optimized SD and FDFs containing domperidone and  $\beta$ -cyclodextrin along with HPMC K15M and gellan gum, it was observed that there was endothermic peak of SD 242.45°C and for FDFs 243.19°C no peak corresponding to melting point of the drug suggesting amorphous form of domperidone in the SD as well as FDFs.

#### XRD analysis

The X-ray diffractograms of domperidone,  $\beta$ -cyclodextrin and optimized SD are shown in Fig. 7. The X-ray diffractograms of domperidone and  $\beta$ -cyclodextrin showed characteristic sharp intensity diffraction peaks at 8°C equivalent values of 12°C, 14°C, 16°C, 18°C, 20°C, 24°C, and 28°C which reflected the crystalline nature of drug.

The optimized SD showed a reduction in peak intensity when compared to the pure drug domperidone which was very negligible. The results showed that the SD converted the drug which processed a strong crystal habit into a totally amorphous one and was supported by DSC. As a result of amorphization and substantial increase in surface area, drug particles acquired high internal energy necessary for their enhancing wetting and dissolution of the FDFs.

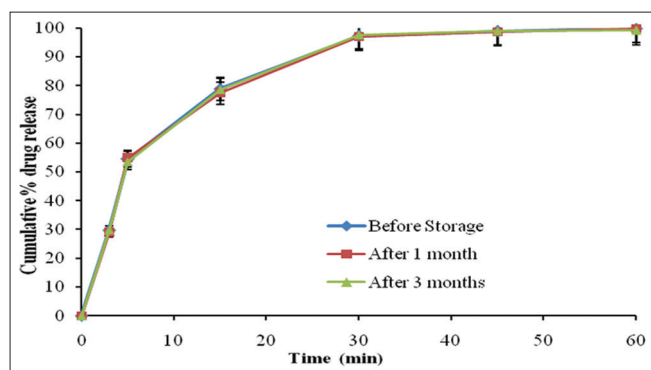
#### Stability studies

The optimized formulation FHG showed good *in vitro* performance when subjected to stability studies. The stability studies were carried out at room temperature on the physical properties, drug content and drug release from the FDFs. The results of these studies are given in Table 11 and Fig. 8. The results thus indicated that there were no visible and physical changes observed in the frequency discrimination even after storage. Weight variation, thickness, surface pH, folding endurance, swelling property, transparency, disintegration time, and elongation were found to be uniform before and after storage at different time period. It was observed that there was no significant change in drug

**Table 11: Stability studies of optimized formulation FHG**

Evaluation parameters	FHG		
	Before Storage	After 1months	After 3months
%Drug Content <sup>a</sup>	98.9±0.88	98.04±0.74	98.69±0.98
Thickness <sup>b</sup>	0.22±0.05	0.21±0.15	0.22±0.09
Weight variation <sup>b</sup>	58.3±0.52	59.18±0.96	57.89±0.88
Surface pH <sup>a</sup>	6.43±0.04	6.45±0.11	6.35±0.16
Folding Endurance <sup>a</sup>	308±0.53	309±0.52	309±0.34
Swelling property <sup>a</sup>	0.86±0.06	0.84±0.04	0.83±0.08
Transparency <sup>a</sup>	Transparent	Transparent	Transparent
Disintegration time <sup>a</sup>	27±0.45	26.0±0.49	27.0±0.34
% Elongation <sup>a</sup>	28.93±0.49	54.65±0.32	25.6±0.96

Where: <sup>a</sup>mean±s.d.(n=3) of domperidone FDFs, <sup>b</sup>mean±s.d. (n=10) of domperidone FDFs



**Fig. 8: Dissolution profiles of optimized formulation FHG on stability**

release from the FHG FDFs. Therefore, the drug release characteristics of FDFs designed were found to be quite stable.

#### CONCLUSIONS

Solid dosage forms that can be dissolved or suspended with water in the mouth for easy swallowing are highly desirable for the pediatric and geriatric population as well as other patients who prefer the convenience of the readily administered dosage form. In present work, the solubility of domperidone was initially enhanced by the kneading method (1:0.5, 1:0.75, and 1:1) using  $\beta$ -cyclodextrin (inclusion). The solubility of domperidone was enhanced by increasing the concentration of  $\beta$ -cyclodextrins, and the complete drug release was achieved 98.86% within 30 min; hence, this ratio is taken for further development of fast dissolving films (FDFs). The FDFs of domperidone were prepared successfully by incorporating the optimized SD SDK3 by solvent casting method using HPMC K15 and gellan gum in different concentrations (10%, 17.5%, 15%, 12.5%, and 20% w/w). From the optimized concentrations of these polymers, another formulation was developed by taking the above two film-forming polymers in combination (5% of HPMC K15 and gellan gum). The FDFs prepared with combination of polymers shown better result when compared with the optimized formulations with individual polymer FH5 and FG5. Solvent casting method was found to be the best approach in the formulation of FDFs. From the study, it was concluded that the formulation prepared with equal compositions of HPMC K15 and gellan gum enhanced the drug release rate. The optimized formulation FHG has been found to be stable. The prepared film also gives benefit in terms of patient compliance, avoids first-pass effect, shows rapid onset of action, increased bioavailability, low side effects and good stability which make these films popular as a novel dosage form. Thus, satisfactory FDFs of domperidone for large scale production are feasible. From the entire study, we can conclude that natural polymers such as gellan gum in single or in combination can be used as film-forming polymer in the formulation of FDFs of domperidone since the primary ingredients are inexpensive, devoid of toxicity, biocompatible, biodegradable, and easy to manufacture.

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#### AUTHORS' CONTRIBUTIONS

Dr. Saripilli Rajeswari the guarantor of this study has designed and supervised the experimental process. Ms. Patibandla Sameera have carried out the experiments and analyzed the results. Dr. K. Hari, Ms. Patibandla Sameera and Ms. Konchada Alekhya have contributed in preparation and revision of the manuscript.

#### CONFLICTS OF INTEREST

All authors have no conflicts of interest.

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