

3D PRINTING OF PHARMACEUTICALS – LEADING TREND IN PHARMACEUTICAL INDUSTRY AND FUTURE PERSPECTIVES

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ABSTRACT

3D printing technology is a rapid prototyping process based on computer-aided design software that is proficient to construct solid objects with various geometrics by depositing numerous layers in a sequence. The major advantages of three-dimensional printing (3DP) technology over the traditional manufacturing of pharmaceuticals include the customization of medications with individually adjusted doses, on-demand tailored manufacturing, unprecedented flexibility in the design, manufacturing of complex and sophisticated solid dosage forms, and economic benefits. Recently, many researchers have been invested their efforts in applying 3DP technology to the pharmaceutical development of drug products and different drug delivery systems. Selective laser sintering, fused deposition modeling, semi-solid extrusion, stereolithography, etc., are the multiple 3DP technologies that can be established in several customized and programmable medicines. Sublingual, orodispersible, and fast-dissolving drug delivery formulations by 3DP technology have been already manufactured. Controlled-release formulations with different characteristics, doughnut-shaped multi-layered tablets with linear release kinetics, and drug-loaded tablets with modified-release characteristics are recently fabricated using 3DP. However, few 3DP methods produce uneven shapes of dosage forms and comparatively porous structures. Cost of transition, adaptation to the existing facility, achieving regulatory approval, etc., are the present challenges that can restrict the extensive application of 3DP technology to pharmaceutical products. Intense research work for modifying the 3DP methods is simultaneously sustained for by-passing the flaws and current limitations of this technology. 3DP technology can act as a convenient and potential tool for the pharmaceutical industry which will set a revolutionary manufacturing style in the near future to facilitate patient-centered health care.

Keywords: Computer-aided design, Three-dimensional printing, Stereolithography, Orodispersible, Fused deposition modeling, Linear release kinetics.

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INTRODUCTION

Drug delivery, a very frequently used and important terminology, belongs to the pharmaceutical sciences. It is the technology used for transporting a compound successively in the body as desired safely to achieve required therapeutic efficacy. New ideas for drug delivery are significantly evolving over the years from the era of conventional oral dosage forms to targeted release drug delivery systems for achieving better patient compliance [1-3]. In the last decade, considerable attention was focused on the development of novel drug delivery systems and patient-centric drug products. Within many discoveries of recent time, three-dimensional printing (3DP) is considered to be the most versatile and revolutionary technology in the pharmaceutical industry [4].

3DP follows additive manufacturing which is a rapid prototyping technology [5]. It is capable to print 3D objects by fusing multiple layers in a particular sequence controlled by computer-aided design (CAD) software [6-9]. Rapid advances in 3DP technology facilitate a wide range of pharmaceutical applications, including advancement in the design of drug delivery systems [10,11]. In the early 2000s, traditional prosthetics and dental implants were first fabricated with the application of 3DP. Now, it can be effectively used at the different stages of drug development process to eliminate the risk of failure [12,13].

Compared to the conventional technologies involved with manufacturing of pharmaceuticals, 3DP possess a lot of advantages such as high amount of drug loading ability, enhancement in productivity, personalization of medications with individually adjusted doses, on-demand production, the ability to fabricate potent drugs with high accuracy and precision, narrow therapeutic window, and cost effectiveness [14,15].

By utilizing the 3D printed drug delivery system, treatment can be customized for multi-drug therapy with the various dosing regimen. This technology can avoid batch-to-batch variation which is very commonly observed in the bulk manufacturing of traditional dosage forms [16,17]. Employment of 3DP technology also supports the development of numerous drug delivery systems such as oral controlled release systems, multi-layered tablets with linear release kinetics, immediate-release tablets, implants, modified release dosage forms, pills, and microchips [18-25]. Moreover, this technology is compatible to wide range of active pharmaceutical ingredients, including proteins, peptides, and poorly water-soluble drugs [26-29].

SPRITAM comprising Levetiracetam as an active pharmaceutical ingredient was the first FDA approved 3D-printed pill [2]. The product was manufactured by utilizing ZipDose technique which is depend on layer-by-layer powder bed fusion system [30].

This review will draw attention toward the significance and future perspectives of 3DP technology in pharmaceutical manufacturing through assessing the impact and implications of the technology. The study is also carried out to explore the different techniques involved with 3DP and to get a thorough outlook of the pharmaceutical products can be fabricated by the method.

DIFFERENT 3DP METHODS FOR PHARMACEUTICAL PRODUCT DEVELOPMENT

Depending on the source of material, energy sources, and other mechanical factors, different 3DP methods have been designed to develop a variety of pharmaceutical products. The different methods for 3D printing are shown in Fig. 1.

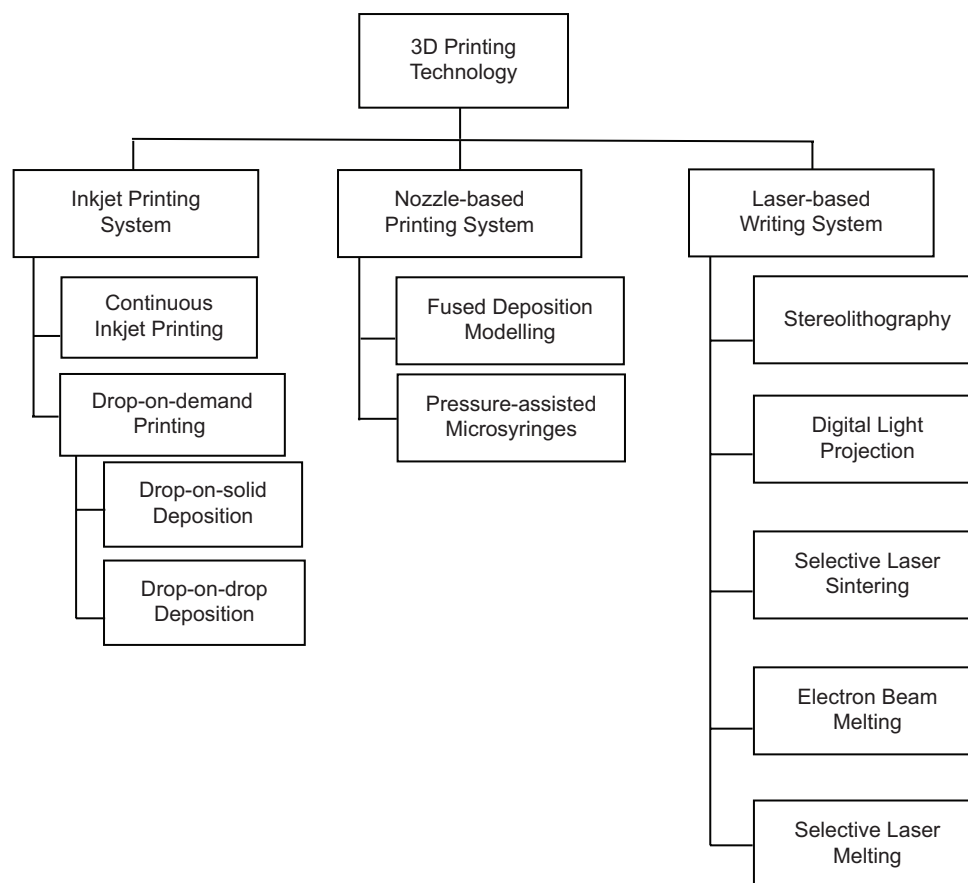


Fig. 1: Categorization of three-dimensional printing technology

Inkjet (IJ) printing system

This system is originated from a similar technique generally utilized for computer-operated inkjet printing. For pharmaceutical implementation of the system, drug solutions are used instead of ink and standard paper with palatable sheets is considered as substrates [31]. This system is classified into two methods, that is, continuous inkjet (CI) printing and drop-on-demand (DOD) printing.

In CI printing, the liquid ink is streamed in a constant flow through an orifice ranging from 50 to 80 μm diameter in the presence of a high-pressure pump. The liquid ink is disrupted into drops at a predetermined speed, size, and specific intervals by applying a piezoelectric crystal. Formation of the electrostatic field is capable to control these parameters [25].

In DOD printing, ink droplets of 10–50 μm diameter with a volume of 1–70 pL are formed [32]. Thermal head and piezoelectric crystal are used as printer heads in the DOD printing. In thermal head of DOD printing, the liquid ink is heated locally at a temperature up to 300°C. It causes formation of bubbles that eject the ink to print. However, application of this thermal head is limited to only volatile liquids. In addition, drugs and pharmaceutical ingredients may be degraded by high vapor pressure for using such a high temperature [7].

When piezoelectric crystal is used for DOD printing, the shape of piezoelectric crystal is changed rapidly that results swift change in volume. An acoustic pulse is created for ejection of the ink [33]. Compared to the thermal head, this piezoelectric crystal in DOD printing can be applied to an extensive variety of liquids. Furthermore, there is no chance of degradation of any drugs since this DOD printing can be functioned at room temperature [7]. Hence, the piezoelectric crystal is more suitable for DOD printing to accomplish pharmaceutical applications [32].

The DOD printing system can be categorized into two subtypes, that is, drop-on-solid deposition and drop-on drop deposition [7]. Drop-on-solid deposition is also known as powder bed fusion, drop on-powder, plaster printing, drop-on-bed deposition, or binder jetting 3DP. This system spreads the solid material in the form of powder on the uppermost portion of a stage which is 200 μm in height followed by spraying a liquid ink as the binder solution on the powders. Then, the stage is pull down, and the specified process is again repeated until the formation of a 3D structure by adhering the consecutive layers [7,34].

The ink droplets of 100 μm diameter are ejected from the printer head onto each other to generate a solid layer in the drop-on-drop deposition method. Thickness of the successive layers is lesser than the ink droplet size and the layers result the formation of a high-resolution 3D structure. This deposition method is proficient of fabricating microscopic drug delivery systems [35,36].

Drop-on-solid deposition system in DOD printing appears to be more applicable for the pharmacoprinting of an extensive range of drugs as compared to drop-on-drop deposition. However, the inkjet printing system enables an important benefit of controlling the dose combination and drug release pattern perfectly [25,37].

Nozzle-based printing system

Nozzle-based printing system has been invented to overcome the limitations of inkjet printing system that includes its applicability to only low therapeutic doses, insufficient hardness, difficulty in multiple layer printing, longer drying time, and formation of a rough surface [25,38]. In nozzle-based printing system, drugs, polymers, and other solid components are mixed with the binder solution. This mixture is then delivered through a nozzle and the subsequent layers are deposited directly to generate a three-dimensional object [39]. This

system can be classified into two methods, that is, fused deposition modeling (FDM) and pressure-assisted microsyringes (PAM) [35].

FDM is one of the most frequently explored 3DP system which is also known as fused filament fabrication [40,41]. In FDM, the drug and thermoplastic polymers are mixed together, followed by incubation in a suitable solvent or melted together, applying hot-melt extrusion technique at an appropriate temperature [42]. Then, the molten mass is extruded into filament using a high-temperature nozzle and the layers formed are deposited on a plate with instant solidification [20]. FDM offers several advantages such as cost-effective manufacturing process, good mechanical strength, ability to modify the drug release kinetics, and fabrication of highly complex therapeutic agents with difficult geometries [32]. FDM printer is capable to fabricate gastroretentive floating 3D-printed tablets by applying hot-melt extrusion after creating the drug-loaded filaments [43]. FDM printing technology has been used to design an enormous diversity of drug delivery systems in the recent development of pharmaceuticals [44-52]. With the several advantages for its pharmaceutical applications, there are also some drawbacks like non-availability of biodegradable thermoplastic polymers which possess good melt viscosity characteristics for their extrusion, high temperature used for extrusion [35].

In PAM, a microsyringe is used to extrude the liquid materials of adequate viscosity [7]. The microsyringe used is capable to move around similar to an inkjet printer head, and the liquid material is released by the aid of compressed air. PAM facilitates in the formation of complex drug delivery systems, microstructured product of 5–10 μm , or less diameter [53]. This method of 3DP involves room temperature to operate in a constant flow. Similar to PAM, another system using piston-assisted microsyringe (PAM2) has been developed to release the printing material through a stepper motor instead of compressed air [54].

Laser-based writing system

This system is based on the theory of photopolymerization, in which free radicals are released upon successful interaction between the photoinitiator and ultraviolet light [14]. Stereolithography (SLA) is a solid freeform fabrication method based on laser oriented printing. A high-energy ultraviolet light beam in the form of a laser is focused and scanned over the uppermost portion of a liquid resin for its controlled solidification by photopolymerization [55]. The polymerized layers are formed and the process is continued until a solid 3D object is found [35]. SLA is a highly accurate technique that produces the 3D object of good surface quality. This method has been already used to create oral dosage forms of paracetamol and aspirin in 5% and 2.5%, respectively, and also widely used in tissue engineering and designing of implants [56,57]. Research studies revealed so many optimistic possibilities of SLA such as fabrication of dosage forms from 28 different drugs in a single print cycle, capability to moderate the drug release pattern from printed products, and production of multi-layered and multi-drug tablets to achieve personalized patient-specific medication [56,58].

Based on the same principle of SLA and digital light projection (DLP), another 3DP method has been developed [59]. As compared to SLA, DLP method offers comparatively faster construction of the 3D object and makes easy to adjust the thickness of polymerized layers [35,60].

Selective laser sintering (SLS) employs the raw materials in powder form and a high power laser is used to melt it followed by fusing of powdered materials together [61]. SLS possesses several advantages such as chemical resistance, speed of printing, and product of higher strength [35]. SLS has been utilized to develop numerous drug delivery systems such as small oral dosage forms with controlled release characteristics, single miniprintlets of paracetamol, and dual miniprintlets of paracetamol with ibuprofen [41].

Electron beam melting and selective laser melting are also some methods, according to laser-based writing system which is broadly used in drug-loaded implants [62].

Three-dimensional bioprinting

3D-bioprinted drug delivery system, a novel approach, has been involved for the treatment of bone fractures and defects. Controlled release of simvastatin through the system for at least 20 days is able to cause bone healing and repairing [63]. A research study effectively proved the efficiency of the system using pectin-based bio-ink to build 3D-bioprinted wound dressings with sufficient antimicrobial activity [64].

Embedded 3DP (e-3DP)

e-3DP, a rapid prototyping technology, in which a deposition nozzle is used to extrude a viscoelastic ink at a predetermined path into a solidifying reservoir. The products are printed by using e-3DP at a temperature 70°C followed by solidification at room temperature. By the alteration of the printing pattern, the dose of printed dosage forms can be changed. This new method of 3DP proved its capability by fabricating chewable tablets with dual drug loading and several oral dosage forms with personalized dosing [65].

There are many other 3DP methods which have been developed, including laminated object manufacturing, stencil printing, multi-jetting modeling, semisolid extrusion printing, and selective heat sintering which are not widely explored for pharmaceutical applications. However, the versatility of the mentioned methods, recent advancement in material sciences, will facilitate different novel approaches toward drug delivery system in the near future [35,41].

FABRICATION OF PHARMACEUTICALS BY APPLYING 3DP

The presently available methods for 3DP technology are majorly involved to fabricate the oral solid and transdermal drug delivery systems. However, research work is continued to discover the possibilities for designing the 3D printing protocol of other drug delivery systems. After the innovation of 3DP technology, it was first applied to fabricate immediate-release tablets containing a single drug. Due to its simple operational technique, FDM was utilized to produce such type of tablets [66-68]. On successful fabrication of the dosage forms, other 3D methods were then also involved for pharmaceutical research and designing of the medicaments.

3DP technology is capable to manufacture the dosage form of complex drugs in a standard and simple way. This technology allows the dosage forms to release the drugs as per need of patients. A wide range of drug release profile for the oral solid dosage forms using single or multiple active pharmaceutical ingredients (polypill) has been successfully developed by applying different methods of 3D printing, as shown in Table 1 [69-82]. High dose (up to 1000 mg) of orodispersible tablets, sublingual, and other fast-dissolving formulations that disintegrate rapidly in the oral cavity has been manufactured using 3D printing [83-86].

3DP-based implants are developed to create complex micro- and macro-structures in a single system. In recent studies, it has been found that multiple drugs can be loaded in the 3DP-based implants to achieve instant therapeutic efficacy, as shown in Table 2 [87-90]. An implant loaded with odd number layers of levofloxacin and even number layers of tobramycin was capable to release the drugs stepwise in a sustained manner for about 2 months. By retaining ideal drug concentration, the drug-device controlled chronic osteomyelitis in rabbits [90]. Nowadays, bone defect can be treated by fabricating scaffolds utilizing 3DP technology through merging the calcium phosphate cement with vascular endothelial growth factor-loaded hydrogel strands [91]. For the treatment of bone tuberculosis, pancreatic cancer, and any other chronic diseases, 3DP-structured multi-drug implants could be a promising approach due to their ideal pharmacological action, site-selective drug release, and cytocompatibility [87,89]. The usefulness of biodegradable implants structured by 3DP technology has been suggested for effective local delivery of anticancer drugs [87].

Table 1: Application of three-dimensional printing in fabricating oral solid dosage forms

Dosage form	Release pattern	API(s)	Three-dimensional printing method used	Reference
Single API tablet	Immediate	Paracetamol	Extrusion	[69]
Single API tablet	Extended	Theophylline	FDM	[70]
Single API tablet	Extended	Prednisolone	FDM	[71]
Single API tablet	Controlled	Pseudoephedrine HCl	Inkjet printing	[72]
Dual compartment tablet	Modified	Rifampicin, isoniazid	FDM	[73]
Single API tablet	Extended	4-aminosalicylic acid/paracetamol	Stereolithography	[16]
Multi-layered tablet	Modified	Acetaminophen	Inkjet printing	[74]
Enteric-coated tablet	Delayed	Paracetamol	FDM	[21]
Gastro-floating tablet	Extended	Dipyridamole	Extrusion	[75]
Single API tablet	Controlled	Ropinirole HCl	Inkjet printing	[76]
Single API tablet	Extended	Fluorescein	FDM	[77]
Caplet	Modified	Paracetamol/caffeine	FDM	[66]
Polypill	Immediate/ Sustained	Aspirin, hydrochlorothiazide, pravastatin, atenolol, and ramipril	Extrusion	[78]
Polypill	Controlled	Captopril, nifedipine, and glipizide	Extrusion	[79]
Bi-layer tablet	Immediate/ sustained	Guaifenesin	Extrusion	[28]
Caplet	Controlled	Budesonide	FDM	[20]
Single API tablet	Controlled	Fenofibrate	Inkjet printing	[80]
Shell-core tablet	Delayed	Theophylline, budesonide, and diclofenac sodium	Dual FDM	[81]
Dual pulsatory tablet	Immediate	Diclofenac sodium	Inkjet printing	[82]

Table 2: Application of three-dimensional printing for developing implants

API(s)	Release pattern	Reference
Poly(lactide-co-glycolide) and polycaprolactone, 5-fluorouracil	Controlled release	[87]
Levofloxacin	Complex drug release	[88]
Isoniazid and rifampicin	Programmed release	[89]
Levofloxacin and tobramycin	Sustained and programmed release	[90]

Table 3: Application of three-dimensional printing for developing microneedles

API(s)	Three-dimensional printing method used	Reference
Rhodamine	Continuous liquid interface production	[92]
Dacarbazine	Multi-material microstereolithography	[93]
Fluorescein	FDM	[94]
Insulin	Stereolithography	[95]
Diclofenac	Three-dimensional printing	[96]

3DP technology facilitates to fabricate sophisticated microneedles of complex geometries. The microneedles formed are uniform in shape, radius of the needle tip is less than 3.5 μm and 400–1000 μm in height [92]. Microneedles fabricated by 3DP have been revealed their potency in the delivery of vaccines, insulin, treatment of skin carcinoma using microstereolithography, trigger finger using microneedle splint, etc., as shown in Table 3 [92-96].

Apart from these applications, fabrication of DNA biosensors with superior selectivity, biomimetic constructs for different stages of drug discovery and development, 3D tissue models, and nanoparticles of controlled size targeting tumor cell has been also reported [13,97].

CURRENT CHALLENGES AND FUTURE PERSPECTIVES OF 3DP TECHNOLOGY

There are few challenges that 3DP technology faces have to be overcome for its wide application in the pharmaceutical industry at a large scale. In the post-processing stage of fabrication, this technology

is unable to produce the product with the desired accuracy. The product also needs a finishing operation like polishing to achieve the final shape. A number of physical and technical parameters related to 3D printing such as thermal conductivity, viscoelastic property, physicochemical characteristics of liquid ink, and printability must be reviewed cautiously [14]. Friability of the dosage forms fabricated by 3DP methods, especially powder bed fusion, is higher as compared to the same produced by conventional manufacturing. The choice of potential raw materials, colorants presently available for 3DP technology, is quite limited as compared to traditional manufacturing processes [25].

SPRITAM is the only 3D-printed product manufactured by Aprelia Pharmaceuticals which got USFDA approval in 2015. However, fulfilling the regulatory requirements for the 3D-printed products in a positive manner will be the obvious way for the extensive pharmaceutical application of this technology at industrial scale [27]. 3DP technology may result massive job loss of a large number of human labor associated with conventional manufacturing processes. Besides this extreme truth, increasing the value of skilled professionals in the field of CAD design, materials engineering, information technology, mathematics, and automation required for the technology will create a huge job prospect.

Based on the ability to print the on-demand personalized dosage forms, it is aimed to convert the current pharmacies into digital pharmacies. To fabricate, the personalized medications as per prescription digital pharmacies can transform the drug-loaded filaments with essential quality which is initially to be developed by the pharmaceutical companies on a large scale. The collaboration between pharmaceutical industry and the digital pharmacies seems to be a conceivable pathway to turn this 3DP technology into reality [98]. The process of manufacturing, transportation, and distribution of medicines to the market by pharmaceutical companies can be replaced by forwarding the formulation databases to the pharmacies for on-demand drug printing. This drastic change in the traditional cycle of manufacturing to distribution seems to be more cost-effective [27].

Endless research work progressed for refinement in 3DP methods may overcome the current technical, physical, and regulatory challenges in the near future [34]. One of the ongoing research studies evidenced some versatile biocompatible raw materials having the ability to modify their characteristics under the influence of external factors. Based on this feasibility, the structural modification has been created, termed as "4D printing" [99,100].

CONCLUSION

Various methods of 3DP technology make it possible to develop highly sophisticated dosage forms with different shapes, allow to fabricate flexible dosages with single or multiple active pharmaceutical ingredients, and offer a wide range of drug release kinetics. 3DP technology is anticipated to play a major role in the movement toward personalized and tailored medications. Rapid advancement and progressed research for 3DP technology will be broadly applicable to the numerous drug delivery systems and accelerate the transformation of pharmacy practice according to individualized medication. It has been noticed that through the flexibility, speed of production, and precision of 3DP, use of the technology for manufacturing and distribution of drugs play a significant role in the current scenario of pharmaceutical industry. However, the pharmaceutical industry has been prepared to percept the fourth industrial revolution with the broad-spectrum manufacturing of customized medicines by 3DP.

AUTHOR'S CONTRIBUTIONS

As this review article is solely authored by Mr. Shankhadip Nandi, Assistant Professor of Gitanjali College of Pharmacy, he is the only person who made a substantial contribution in conception of this topic, procurement, and understanding of the information in the article. Completion of literature review followed by drafting and reviewing the article judgmentally, necessary revisions required as per reviewers' comments have done by the author. He has given final approval of the version to be published.

CONFLICTS OF INTEREST

The author confirms that there are no such conflicts of interest to publish this review article.

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