

Original Article

## NANOSTRUCTURED LIPID CARRIERS (NLCs): A PROMINENT TOPICAL DELIVERY SYSTEM FOR COENZYME Q<sub>10</sub> AND MYRICA ESCULENTA LEAVES EXTRACT FOR ANTI-AGING POTENTIAL

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### ABSTRACT

**Objective:** In this study, *Myrica esculenta* (ME) leaves extract along with Coenzyme Q10 was entrapped in nanostructured lipid carriers (NLCs). The formulation variables were successfully optimized using 2<sup>3</sup> factorial design.

**Methods:** Preparation of NLC was carried out by solvent injection technique. The formulation of NLC was consisting of the methanolic extract of *Myrica esculenta* leaves and Coenzyme Q10 as key ingredients. Oleic Acid (OA) was taken as liquid lipid, Precirol ATO 5 (PATO) as solid lipid, and Poloxamer 407 (P407). The formulation variables were statically optimized using 2<sup>3</sup> factorial design, followed by the characterization of the formulation.

**Results:** The results demonstrated that the best optimized NLC formulation F5 of Coenzyme Q10 and plant extract exhibited the smallest size 169.46 nm and highest entrapment efficiency 90.06±0.171 %. Furthermore, it showed good physical stability at 28 d after preparation.

**Conclusion:** The developed NLCs of Q10-ME extract from this study could be explored as the effective anti-aging formulation.

**Keywords:** Anti-aging cosmetics, Antioxidant activity, Factorial design nanostructured lipid carriers

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### INTRODUCTION

The human being of the modern world had a great inclination to search for an everlasting youth. In this physical world facial appearance became a crucial factor to influence social relations in many situations due to which people tend to judge personality based on facial manifestation [1]. This desire had ultimately triggered for the development of new products, methods and technology in the cosmeceutical industry which might revert back the clock [2]. Skin is the largest human organ contributing, a major target of oxidative stress [3]. Skin aging is a gradual deterioration of the physiological functions of skin which results in wrinkles or loose skin that causes unattractive appearances. Several theories have been laid down to describe the mechanism of the skin aging of which the most successful and referred is the free radical theory based on oxidative stress [4].

Many antioxidant agents have been studied to develop novel anti-aging products. Coenzyme Q10 one of the most popular antioxidants, naturally occurring in the skin that had been studied in this field [5] most common products composed of CoQ10 generally contained in the range of 0.5–1.0% in anti-wrinkle products as well as in anti-oxidant products. It is having the tendency to show the adverse effect at higher doses if taken orally [6].

To solve this problem lipid-based nano-particulate drug carriers have been developed to increase solubility and improve the bioavailability of poorly water soluble and/or lipophilic drugs [7]. The plant extracts usually contain polyphenols such as flavonoids, which react with reactive oxygen species (ROS) to neutralize the harmful effects of free radicals [8].

*Myrica esculenta* Buch.-Ham. (Myricaceae) commonly known as Box Berry, Kaiphal, and Katphala in Ayurveda is widely used treatment of gulma (abdominal tumors), jvara (fever), arsa (piles), grahani (irregular bowel function), pandu roga (anemia), hrillasa (nausea), mukha roga. The medicinal properties of *M. Esculenta* are well known as per ethnobotanical surveys. Therefore in present study researcher had made an attempt to develop topical drug delivery system which may enhance the potency of Coenzyme Q10 by incorporating methanolic extract of *M. esculenta* into NLC carriers to offer a great

potential to justify the objectives of present work [9]. Considering these aspects, researchers have selected NLCs as carriers due to their special nanostructures which tend to improved properties for therapeutic loading, better drug release profile and stability [10].

### MATERIALS AND METHODS

Coenzyme Q10 (CoQ10) was purchased from Sigma-Aldrich Chemicals, St. Louis, MO. Precirol ATO 5 (PATO), Oleic Acid (OA) and Poloxamer 407 (P407) were provided as gift samples from Gattefossé Saint-Priest, France and BASF Corporation, USA respectively. All other chemicals and reagents used were of analytical grade and procured from SD Fine Chem Limited, Mumbai. The plant specimen, i.e. dried leaves of *M. esculenta* were collected from the northern Himalayan region of Garhwal Uttarakhand, India in the month of March 2015 from the height of 1685.53 Meters N 29.8688 ° N, 78.8383 ° E. The plants were identified and authenticated in BSI, Allahabad, India (voucher specimen BSA-94627). The Standardization of plant extract was carried out through HPLC method followed by quantification of gallic acid in *M. esculenta* extract using RP-HPLC. The NLCs were prepared through the solvent injection technique and statically optimized by 2<sup>3</sup> factorial design [11-12].

### Standardization of plant extract through HPLC method

*M. esculenta* methanolic extract was standardized through reverse-phase high-performance liquid chromatography (RP-HPLC). Lyophilized hydro-alcoholic extract of *M. esculenta* was accurately weighted and volume of the solution was adjusted in a volumetric flask to obtain a final concentration of 1 mg/ml. The optimized mobile phase consisted of acetone with 1% acetic acid in water in the ratio of 76: 24 (v/v) with the flow rate of 1 ml/min. The HPLC system comprised of rheodyne-7725 injection valve with a sample loop (20 ml), Vacuum degasser, quaternary pump and photo-diode array detector (PDA) was used, with data acquisition by Empower TM 2 software (Waters 600, Milford, MA, USA). Chromatography was performed on a Spherisorb C18 column (250 mm × 4.6 mm, 5 mm; Waters, Ireland) fitted with a C18 guard column (10 × 3.0 mm). The sample elution was performed at 25 °C and detected at the UV

wavelength of 254 nm. A sample was analyzed by HPLC using 20  $\mu$ L injection volume of a syringe (Hamilton Microliters; Switzerland). The pH meter (Orion 3 Star, Thermo-Scientific) was used to adjust the pH of the mobile phase. Amount of the marker compound present in the crude plant extract was determined through the calibration curve. Calibration curve constructed by the corresponding peak area of the gallic acid as standard was plotted against the concentration of standards by means of linear regression. The stock solution of a standard compound was prepared by dissolving the known amount of gallic acid in methanol at a concentration of 1 mg/ml.

#### Quantification of gallic acid in *M. esculenta* extract

*M. esculenta* extract was standardized by RP-HPLC under the isocratic conditions using the external standard calibration

technique. A bioactive compound was identified by comparing with the respective retention time (Rt) of the gallic acid as standard. The calibration curve was plotted by plotting peak areas against concentrations and five standard marker ranges from 100–500  $\mu$ g/ml. The standard compound shows a good linearity between concentrations and the peak area, with the correlation coefficient ( $r^2$ ) of 0.998.

Obtained chromatograms from HPLC analyses of the extract and their respective markers are shown in fig. 1. The optimum separation of was achieved by using the mobile system at the volume ratio of acetone with 1 % acetic acid in water in the ratio of 74: 24 (v/v) with a flow rate of 1 ml/min. The retention time of gallic acid was found to be 4.013 min. The percentage amount of standard constituent (gallic acid) present in the crude extract was found at 1.64% (w/w).

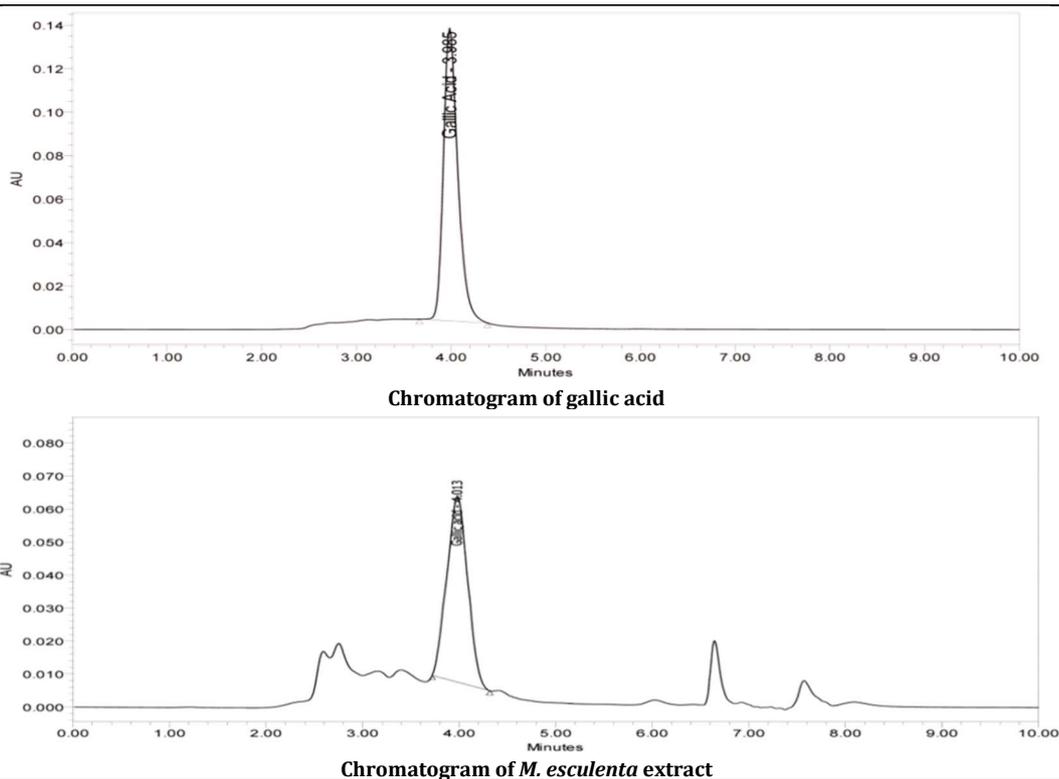


Fig. 1: RP-HPLC chromatograms of gallic acid and *M. esculenta* extract

#### Excipient compatibility test

Excipient compatibility test was carried out for 21 d by taking the physical mixture in 1:5 ratio of CoQ10 separately with PATO, OA and P407 respectively at temperature  $40 \pm 2$  °C and relative humidity  $75 \pm 5\%$ .

#### Experimental design of NLCs

In this study,  $2^3$  factorial design was used to optimize NLCs. In order to optimize, the amount of solid lipid, (PATO,  $X_1$ ), amount of liquid lipid (OA,  $X_2$ ) and concentration of surfactant (P407,  $X_3$ ) were selected as independent variables. Each factor was set at two levels +1 and -1. The actual values and coded values of different variables are given in table 1. Eight formulations of NLCs (F1-F8) were prepared according to design. The particle size and % entrapment efficiency were taken as response parameters.

#### Evaluation of response parameters of NLC

##### Particle size and zeta potential

The particle size and the zeta potential of the formulations were measured using Malvern Zetasizer. The polydispersity index (PDI) was used as a parameter of the size distribution. The samples were

diluted with double distilled water prior to particle size and zeta potential determination at 25 °C.

##### Entrapment efficiency

The percent entrapment efficiency of the CoQ10-ME loaded NLC was calculated by using the equation reported by Shah and Pathak, 2010 [13] and %EE was calculated by the following equation:

$$\%EE = [W_a - (W_s + W_p)]/W_a$$

Where  $W_a$  is the amount of drug added in the system,  $W_s$  is the amount of drug in the supernatant after centrifugation, and  $W_p$  is the amount of drug in the purification medium.

##### Drug content determination by HPLC

Estimation of gallic acid (GA) content in the formulations was analyzed by HPLC. (The standard stock solution was prepared by dissolving the known amount of GA in methanol to get a concentration of 1000  $\mu$ g/ml. Different aliquots were prepared by subsequent dilution with the same solvent. Samples were stored at 4 °C and protected from light before using. In this analysis, the mobile phase of acetonitrile and deionized water was used as a proportion

of 35:65, 30:70 and 25:75 v/v (1% glacial acetic acid; pH 2.2) which were sonicated for 15 min and degassed prior to use. Before applying all samples were also filtered through 0.45  $\mu\text{m}$  (NYL) syringe filter. The recoveries of standard compounds from various samples and formulation at three concentration levels were

determined by measuring the percentages of detecting concentrations over additional concentrations. The quantitative analysis was repeated about three times ( $n=3$ ) by comparing and interpolating the peak area (response) of the sample with the standard.

**Table 1: Formulation of NLC of Q<sub>10</sub>-ME using 2<sup>3</sup> factorial design**

Formulation code	Amount of CoQ10 and plant extract (1:1)	Amount of pato (X1)	Amount of OA (X2)	Amount of P407 (X3)	Response parameter
F1	10	-1	-1	-1	Particle size percentage entrapment efficiency
F2	10	+1	-1	-1	
F3	10	-1	+1	-1	
F4	10	-1	-1	+1	
F5	10	+1	+1	-1	
F6	10	+1	-1	+1	
F7	10	-1	+1	+1	
F8	10	+1	+1	+1	
F9	10	-0.098	-0.834	+0.187	

Where: X1:-1= 0.5% and+1= 2.5% w/w; X2:-1= 0.10% and+1= 0.30% w/w; X3:-1= 0.80% and+1= 1.2% w/v

### Statistical analysis

The effect of independent variables on the responses was modeled by Design Expert software version 11 (Stat-Ease, Inc., Minneapolis, USA). Polynomial equations were generated for the dependent variables that were reduced by removing non-significant coefficients by applying one way ANOVA. Level of significance was set at  $p<0.05$  [14].

### Validation of experimental design

The experimental design was validated by an extra checkpoint formulation (F9) [15]. The predicted values for particle size and entrapment efficiency for F9, generated by their respective polynomial equations were compared with experimental values and tested for statistical significance using pooled t-test at 95% confidence interval, and degree of freedom = 3 ( $p<0.05$ ) [16].

### Selection of the optimized formulation

Optimized formulation was selected on the basis of the desirability factor as calculated by the Design Expert software version 11 (Stat-Ease, Inc., Minneapolis, USA).

### Visualization by transmission electron microscopy

The morphology of selected CoQ10 ME loaded NLC dispersion was observed by transmission electron microscopy. One drop of the CoQ10 ME loaded NLC dispersion was spread on a carbon-coated copper grid and the excess droplets were removed with filter paper.

A drop of 4%w/v phosphotungstic acid solution was dropped into the grid. The negatively stained sample was air dried at room temperature and examined at 15000X magnification.

### Stability studies

Stability of the selected optimized NLCs dispersion was determined as per ICH guidelines for 28days Effects of temperature and relative humidity on physical changes, particle size, and drug content was studied for NLC dispersion [17].

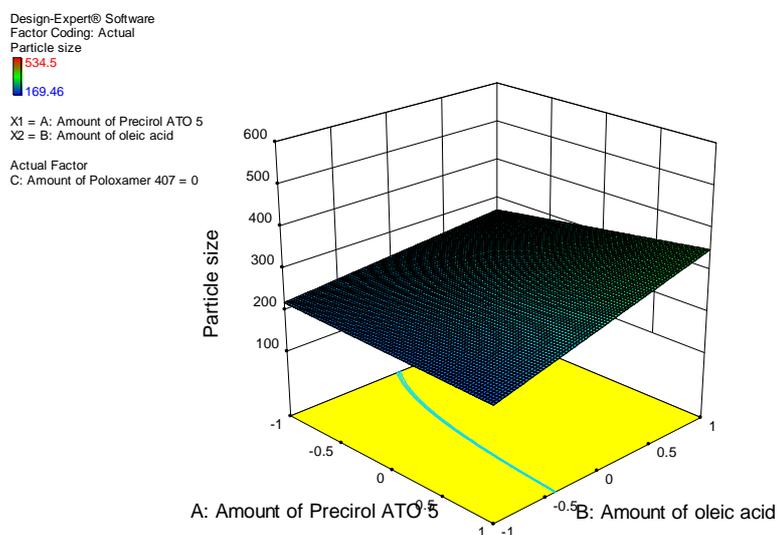
## RESULTS

### Drug-excipient compatibility

Drug-excipient compatibility was determined by the binary mixture method. After 21 d no physical change was observed. The drug content was found out to be 97.25, 96.46 and 98.62 % for physical mixture PATO, OA and P407 respectively. Thus it could be said that the excipients selected for the formulation are safe and have no impact on the efficacy of the product. Furthermore, it is supported with the help of interaction plots obtained by the statistical design (2<sup>3</sup> factorial design).

### 2<sup>3</sup> Factorial design

The factorial design was used for optimization of CoQ10-ME loaded NLC as it is an effective tool for optimization of independent variables. Thus, formulation F1-F8 were prepared according to the factorial design and evaluated for the dependent variables.



**Fig. 2: Response surface plot for particle size analysis**

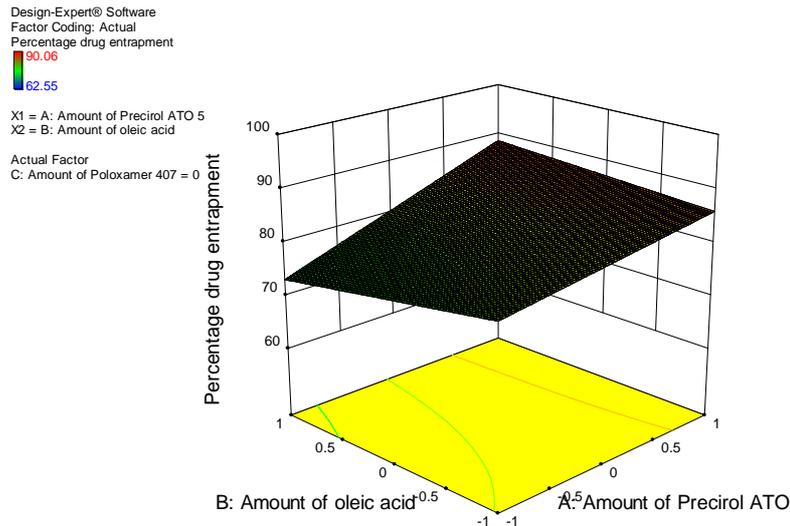


Fig. 3: Response surface plot for analysis entrapment efficiency

### Preparation of nanostructured lipid carriers

NLCs were prepared by solvent injection technique that is based on rapid diffusion of the solvent across the solvent-lipid interface with the aqueous phase [18]. Thus, the diffusion rate of the organic solvent through the interface seems to be a critical parameter for the particle size determination. The major limitation with NLCs is its separation due to their small size and low density of the lipids. To overcome this limitation, in the present study, the pH of the dispersion was reduced to 1.5–2 to adjust the zeta potential for aggregation of NLCs and facilitate the centrifugation and consequently separation.

### Particle size and zeta potential measurements

Values of the particle size and surface charge of the developed NLCs are shown in table 2. The results showed that the amounts of PATO

and OA were critical parameters governing the particle size. After production, the mean diameters of the particles were in the range of 165.9 ~226.8 nm, depending on the lipid loading, and polydispersity was <0.45. Upon increasing the OA percentage in the lipid matrix from 0.10% to 0.30% w/w, the mean particle size decreased. F5 exhibited the smallest size among all the formulations tested. As depicted in table 2, the zeta potential value of the lipid nanoparticles was negative.

### Drug entrapment efficiency

An important issue with respect to the use of nanoparticles as drug carriers is their capacity for drug loading. The effects of OA concentration on drug entrapment efficiency of NLC were investigated. It is clear that the drug entrapment efficiency of nanoparticles increased from 80.63 to 94.50% respectively, with increasing the percentage of OA from 0.1 to 0.3 % by weight (table 2).

Table 2: Physical characterization of CoQ10-ME NLCs

Formulation code	Particle size (nm)	PDI <sup>a</sup>	Zeta potential <sup>a</sup> (mV)	%EE <sup>a</sup>
F1	176.52±0.12	0.243±0.09	-30.01±0.31	80.61±0.62
F2	214.18±0.31	0.261±0.21	-31.39±0.52	85.58±0.43
F3	288.57±0.65	0.263±0.10	-30.02±0.46	62.55±0.49
F4	264.58±0.17	0.267±0.74	-28.08±0.17	79.64±0.22
F5	169.46±0.58	0.212±0.17	-36.39±0.08	90.06±0.17
F6	197.27±0.09	0.249±0.45	-31.89±0.24	86.45±0.36
F7	254.2±0.16	0.243±0.76	-33.45±0.78	83.97±0.41
F8	534.5±0.27	0.384±0.08	-28.51±0.09	87.43±0.35
F9(P)	226.25±0.10	0.267±0.14	-31.28±0.11	82.64±0.52
F9(E)	226.11±0.29	0.258±0.35	-31.35±0.34	82.55±0.41

P= Predicted, E= Estimated, a= mean±SD, n = 3.

### Statistical analysis

Statistical analysis was done by Design expert software version 11 (Stat-Ease, Inc., Minneapolis, USA) and the second order polynomial equations were derived. The transformed equations are,

$$\text{Particle size} = 264.41 + 16.41X_1 + 49.27X_2 + 50.23X_3 + 23.86X_1X_2 + 36.81X_1X_3 + 32.44X_2X_3 + 63.05X_1X_2X_3$$

$$\text{Percentage drug entrapment} = 82.04 + 5.34X_1 - 1.03X_2 + 2.34X_3 + 2.40X_1X_2 - 2.78X_2X_3 + 2.36X_1X_3 - 3.24X_1X_2X_3$$

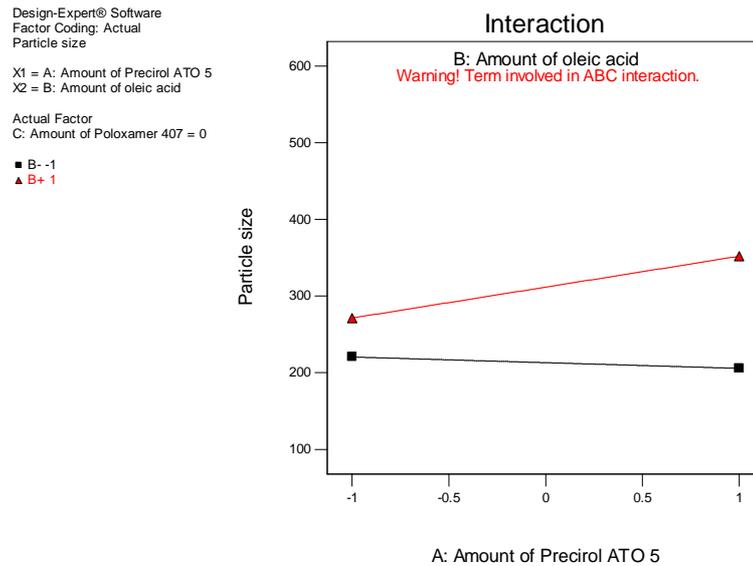
Where X1, X2, and X3 are the independent variables. The effects of various independent variables on the dependent variables are

illustrated in fig. 2 and fig. 3 that clearly depicts the effect of varying the levels of independent factors on dependent factors.

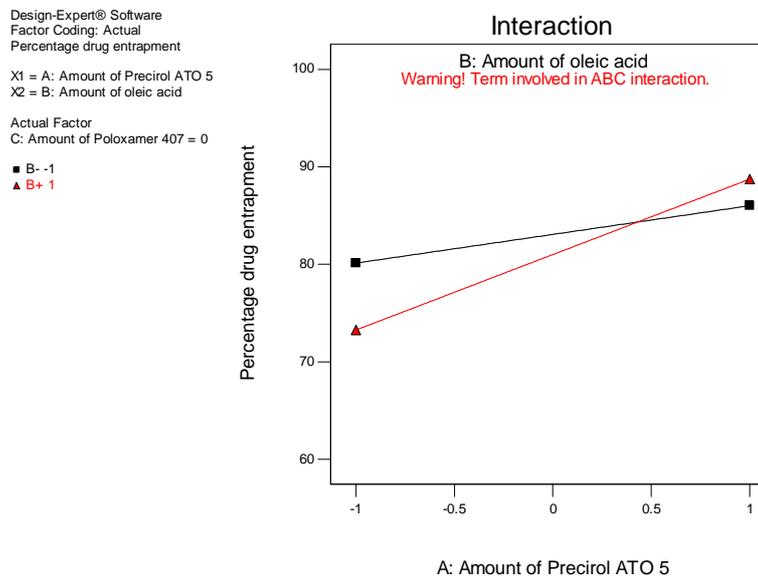
These polynomial equations were utilized for validation of the experimental design. An extra design checkpoint formulation (F9) was prepared. Calculation of the predicted value(s) for particle size and % EE were made and compared with the experimental values as determined by evaluating F9. Close resemblance between predicted and experimental values indicated the validity of the generated model.

### Assessment of interaction in independent variables

The possible excipient interaction was analyzed with the help of graphs obtained by the statistical design, for each response parameter(s), which in turn indicates the significance of experimental design (fig. 4 and fig. 5)



**Fig. 4: Interaction between independent factors and particle size**



**Fig. 5: Interaction between independent factors and entrapment efficiency**

### Validation of the experimental design

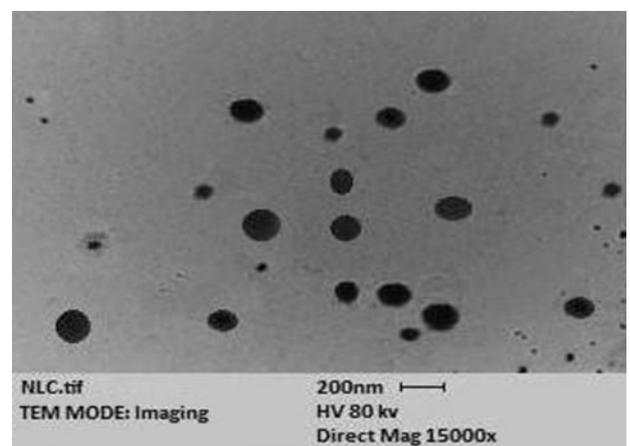
An extra design checkpoint formulation (F9) was made and the predicted value and experimental values of dependent variables were compared using pooled t-test at 95% confidence interval, a degree of freedom 3 and  $p < 0.05$ . No significant difference was recorded between the two values (table 2) thereby establishing the validity of the generated model.

### Selection of optimized formulation

Eventually, F9 with desirability factor = 1, the particle size of 226.11 nm and entrapment efficiency of  $82.55 \pm 0.41\%$ , was identified as the optimized formulation.

### Transmission electron microscopy

Transmission electron microscopic image of NLC indicated spherically shaped particles with narrow size distribution. No aggregation was observed as shown in fig. 3.8. As viewed, all the particles were less than 200 nm, a size particularly suitable for topical delivery.



**Fig. 6: Transmission electron microscopy of NLC formulation F5**

### Stability studies

Stability of the selected optimized NLCs dispersion was determined as per ICH guidelines on the basis of effects of temperature and relative humidity on physical changes, particle size, and drug content was studied for NLC dispersion. The drug content found out to be 98.16 %, 95.49 and 93.38% on subjecting the formulation for 28 d at 25±2 °C temperature 60±5% RH, 30±2 °C temperature 65±5% RH and 40±2 °C temperature 75±5% RH respectively. At the end of the study, there was no any sign of physical change or deformity.

### DISCUSSION

The results of the experimental design were analyzed using Design Expert software. The selected independent variables like the amount of PATO, amount of OA and concentration of P407 had significantly influenced the particle size and, % EE that is very much evident from the polynomial equations. The possible interactions between X1X2, X2X3, and X1X3 for each response were also investigated (fig. 4 and fig. 5).

Graphically, the interactions are visualized by lack of parallelism in the lines, for each response parameter(s) indicated interactions. The response surface plots (fig. 2 and fig. 3) generated using polynomial equations represent a simultaneous effect of any two variables on response parameter taking one variable at a constant level. On carefully observing these plots, the qualitative effect of each variable on each response parameter can be visualized.

### The effect of each independent variable was observed on these dependent variables and the following conclusions were drawn

In increasing the amount of PATO, the particle size increased, indicating that the particle size is highly dependent on the amount of lipid used. On increasing the lipid content the viscosity of the lipid-solvent phase increase resulting in the reduction in the diffusion rate of the solute molecules to the outer phase that results in an increase in particle size. But as observed in table 2 the increase in particle size leveled at 2% w/w of PATO and on further increase in the amount of PATO, the particle size decreased.

The abundance of lipid results in diffusion of lipid to the outer core of NLC resulting in a decrease in particle size. In addition to particle size, the lipid content also affected the entrapment efficiency. An increase in the amount of PATO resulted in an increase in % EE increase, higher Precirol content means availability of more amounts of the triglycerides containing a binary mixture of tripalmitin and tristearin, act as solubilizing agents for the lipophilic drug(s) [19].

Careful analysis of the experimental design revealed that the liquid lipid, oleic acid as another major component that affected the particle size of NLCs. As indicated by factorial design, the particle size decreased while moving from lower level to higher level of OA. Thus when the amount of OA increased from -1 level to +1 level, the particle size decreased from 534.5 nm to 169.46 nm.

The third independent variable, P407 was also varied at different levels using factorial design and its effect on particle size was analyzed. At the lowest level, the particle size was 214.18 nm (formulation F2) that dropped to 197.27 nm (formulation F6) at the highest level of P407 indicating that increase in the amount of poloxamer can cause a decrease in particle size.

Increase in P407 causes a surfactant induced reduction in surface tension and prevents aggregation of the particles consequently leading to a decrease in particle size. Similarly, the percent entrapment efficiency was observed to decrease from 90.06±0.171 % to 87.43±0.359% as we moved from -1 to +1 level of surfactants.

According to our criteria of lower particle size, higher % EE, and higher desirability factor, F9 was selected as optimized formulation (desirability value of 1.0). Consequently, the coded optimized level for the amount of PATO, amount of OA, the concentration of P407, were identified as -0.098, -0.834, and +0.187, respectively. These coded optimized values can be converted to actual optimized values by using principles of transformation by use of the following equation [20].

$$\text{Coded Value (x)} = \frac{\{\text{Actual value of X} - \text{Average of the actual level}\}}{0.5 \text{ difference between the actual level}}$$

Transmission electron microscopic image of optimized NLC indicated spherically shaped particles with narrow size distribution. No aggregation was observed as shown in fig. 6.

### CONCLUSION

Nanostructured lipid carrier of Coenzyme Q<sub>10</sub> and *M. esculenta* leaves extract were successfully developed and statistically optimized by using 2<sup>3</sup> factorial design. The obtained NLCs were nanosized particles with high entrapment efficiency. The enhanced permeation of the drug through NLC carriers might help in enhancing the pharmacological efficacy of CoQ<sub>10</sub>, subsequently enhancing the anti-aging potential of CoQ<sub>10</sub> with polyphenolic herbal extract of *M. esculenta* leaves. The statistically optimized CoQ<sub>10</sub>-ME NLC carriers containing GA may prove the prominent and enhanced antiaging potential of CoQ<sub>10</sub>.

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### AUTHORS CONTRIBUTIONS

All the author have contributed equally

### CONFLICT OF INTERESTS

The authors declare no conflict of interest

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