

Review Article

NANOTECHNOLOGY FOR DETECTION OF DISEASES CAUSED BY VIRUSES-CURRENT OVERVIEW

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Received: 24 Nov 2020, Revised and Accepted: 03 Feb 2021

ABSTRACT

Nanotechnology is having a high impact on the development of a novel class of biosensors called nanobiosensors. This technology has utilized some extremely exciting elements for sensing phenomenon improvement. The utilization of nano-materials, nano-rods, nano-particles, nano-tubes have aided rapid, reliable reproducibility and its detection in a much better way. The unique properties of nanobiosensors and its varied applications have influenced biosensing research. Since longtime, nanobiosensors have been utilized worldwide for the diagnosis of diseases co-related with molecular detection of biomarkers. This paper highlights the use of such nanobiosensors for the detection of the virus, infections, fungal pathogens, Human Immunodeficiency Virus (HIV) related diseases such as Cardiovascular diseases (CDVs), Renal Arthritis (RA) through different techniques including electrochemical biosensing, optical biosensing, point of care-diagnostics etc.

Keywords: Nanobiosensor, Disease diagnosis, Voltammetry, Amperometry, Point of care testing

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INTRODUCTION

Viruses are the tiniest parasites which have the capability in affecting the physiological behaviour of the host in which they enter and infect. Several living species such as bacteria, plants, human beings and animals are the host of these viruses. Viruses are adaptable and their modes of action are varied; due to this greater number of deaths are occurring in the entire globe, especially because of the human immunodeficiency virus (HIV), Zika virus (ZIKs), influenza infections etc. The transmutation of the existing known viruses currently leads to epidemics, most probably when such mutation occurs at the single level of nucleic acid it may be fatal for the human population. Thus, early diagnosis of these viruses is of high importance for improving the patient's quality of life. Varied conventional approaches are available for the detection of viruses and their interaction in developing infections [1]. Biosensors and nano-bio sensors are one of the conventional methods for the detection of such viruses. Since a long time, the use of biosensors has been one of the fastest technologies due to its varied applications. A biosensor is defined as a device which is designed for detection and quantification of a biochemical molecule for example DNA sequence, antibodies, enzymes, immunological molecules or proteins. Biosensor device consists of three components viz; bioreceptor (analyzes the material), transducer (converts signal) and detector (gives response). Later, nanotechnology showed exciting ingredients for the improvement of the biosensing phenomenon, this technology developed a novel class of biosensors named as nano-biosensors. The high sensitivity of nano-bio sensors is one of the potential benefits for its detection over conventional methods [2].

Nanobiosensors are defined as the devices that are used for measurement of a biological or biochemical event by using any magnetic, optical or electronic technology through a compact probe. Due to the utilization of several nanomaterials such as nanoparticles, nanorods, nanotubes and nanowires this device enables faster detection and its reproducibility in a better way. High surface area nanomaterials are useful in producing nano-bio sensors with shorter response times and greater sensitivity. Selenium nanoparticles (SeNPs) are also being used for various therapeutic applications such as antioxidant, anticancer and antimicrobial etc [3]. The nanostructures present in nano-biosensors act as an intermediate layer in between physicochemical detector components and

biological agents, with nanomaterials a transducer is combined to construct a biosensor. Nanobiosensors are classified in a varied diverse area for their sensing mechanism, such as optical, electrochemical, mechanical and calorimetric. Fig. 1 depicts the different variations and types of nanobiosensors. A nanobiosensor is majorly used to detect several biological agents, such as nucleic acids, pathogens, antibodies and metabolites. Nanobiosensors has varied applications ranging from the estimation and diagnosis in the *in vivo* aspects of the healthcare industry, environmentally monitoring toxicants, pollutants and physical aspects like heavy metal toxicity, humidity, etc. Recently in one of the articles it is revealed that nanovaccines and nanobots are also under consideration for the treatment of most of the diseases [4]. Considering the advantages of these nanobiosensors, in current review, we will summarize different types of nanobiosensors developed so far for the detection of viral diseases [5].

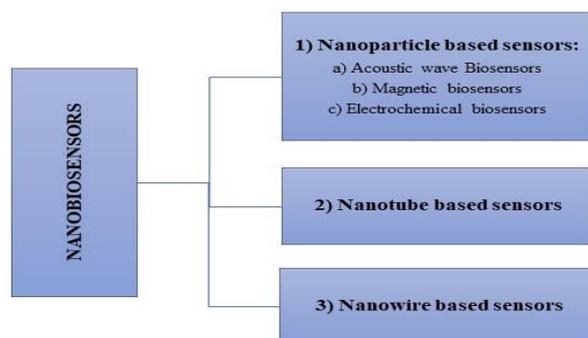


Fig. 1: Nanobiosensors types and variations

Search criteria

The selection of articles for the current review were searched by using keywords in certain specialized databases such as Elsevier (Science direct), Pubmed Medical subject headings (MeSH) and Medline. The keywords which were utilized are terms that were related to

nanobiosensors and its diseases such as; "Nanobiosensors used for detection of viral diseases" OR "Viruses detected through nanobiosensors". Articles displayed on specialized databases were screened manually on basis of their title and abstract. Irrelevant and duplicate documents were excluded and those articles that met the inclusion and exclusion criteria were included in this study. Inclusion of these studies was based on the following criteria: (a) in a peer-reviewed journal it should be an original publication; (b) nanobiosensors should

be utilized for the detection of diseases related to viruses. Only those articles which were written in English and published till now i. e; 2020 were reviewed. Exclusion criteria, were articles which are not applied to pharmaceutical field and those articles which were written in any language other than English, duplicates etc. After filtration and screening, 52 studies published between 1996-2020 met the inclusion criteria and these were included in the review. The selection strategy of review articles which were included is portrayed in the flow chart (fig. 2).

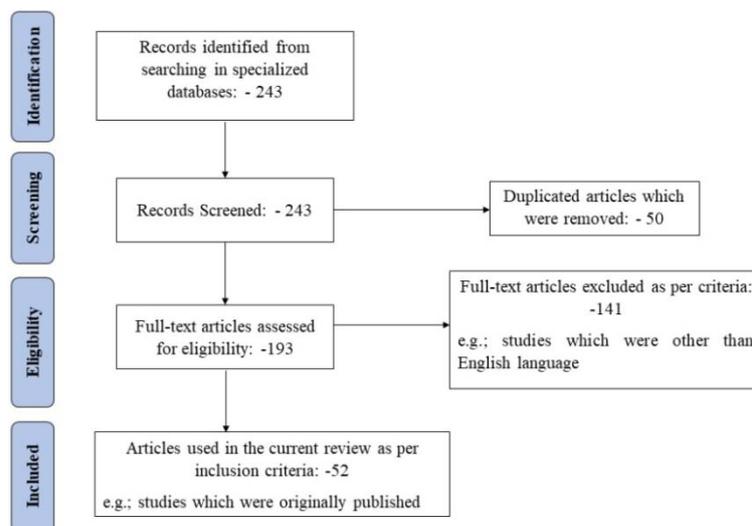


Fig. 2: Flow chart of the selection strategy of articles included in the review

Overview of electrochemical nanobiosensors

Biosensors based on nanomaterials have been utilized for the detection of biological molecules in the entire world. It is an evolving field where the interrogation of the electrochemical nanobiosensors is utilized in the form of impedance, current and potential. When there is a change in the signal response, the biological recognition event with high sensitivity and selectivity occurs. This type of biosensors is also utilized for the detection of glucose and are used

with the combination of varied analytical techniques with their specificity of the desired analyte, such as conductometry, potentiometry, voltammetry etc. Due to the rapid detection and outstanding results through nanobiosensors these are used worldwide for detection of virus in disease diagnosis compared to conventional methods, such as RT-PCR, ELISA which are expensive and require more time [6]. Table 1 gives a glimpse of detection values, linearity range, nanomaterials used and detection method by Electrochemical nanobiosensors for diagnosis of diseases.

Table 1: Overview of electrochemical nanobiosensors in viral diseases

Detection method	Nanomaterial	Limit of detection	Linear range	References
EIS	Indium tin oxide electrodes	2-3 ng/ml	1-1000 ng/ml	[7]
glip-T	1,6-Hexanedithiol and chitosan stabilized gold nanoparticle	0.32±0.01 x10 ⁻¹⁴	1x10 ⁻¹⁴ -1x10 ⁻² M	[8]
DNA hybridization	Electrospun semi-conducting Manganese (III) Oxide (Mn ₂ O ₃)	120 x 10 ⁻²¹ M	-	[9]
SWCNTs	Nanotubes	10 ² CFU/ml	10 ² -10 ¹⁰ CFU/ml	[10]
EIS	Mercaptopropylphosphonic acid functionalized copper doped zinc oxide nanofibers	6 ag/ml	10 ag/ml-10 µg/ml	[11]
Amperometry	Silver graphene quantum dots (Ag/GQDs)	1ZM	1µM to 1ZM	[12]
Voltammetry	Nanoprobes	4 pg/ml	4-53 pg/ml	[13]
Nanoporous membrane-based nanobiosensor	5' aminated DNA probes	9.55 x 10 ⁻¹² M	10 ⁻¹² to 10 ⁻⁶ M	[14]

EIS-Electrochemical impedance spectroscopy, SWCNTs-single-walled carbon nanotubes, CFU-colony forming unit, ag-attogram, µg-microgram, ZM-zepto molar, µM-micro-molar

Electrochemical methods

Electrochemical nanobiosensors are the most common biosensors widely developed and utilized due to its several applications in agricultural, and especially in clinical applications and for industrial analysis. These biosensors generally provide several advantages ranging from high specificity of their biological recognition process,

better specificity, low background noise, cost-effectiveness, rapid detection and better signal-to-noise ratio. Due to these varied applications and advantages, Electrochemical nanosensors are utilized for early detection of disease-related biomarkers [15]. Lin et al. (2018) designed a 3D nanostructured indium-tin-oxide (ITO) electrodes, immobilized it with toll-like receptor proteins (TLRs) for detection of the microbial pathogen components. Results revealed a linear dynamic

range of (>10⁴) and magnitude lower detection limits of (2-3 ng/ml of the microbial component) with 30 times better sensitivity for lipopolysaccharide and flagellin when compared with planar gold and ITO-based TLR sensors using TLR-based Electrochemical impedance spectroscopy (EIS) biosensors [7]. Bhatnagar *et al.*, (2018) developed 1,6-Hexanedithiol and chitosan stabilized gold nanoparticle-mediated self-assembly of glip probes (glip-P) on gold electrode-based electrochemical biosensor for diagnosis of Invasive Aspergillosis, which is caused by *Aspergillus fumigatus*. The limit of detection of this biosensor was calculated to be as $0.32 \pm 0.01 \times 10^{-14}$ (RSD < 5.2 %) within a dynamic range of 1×10^{-14} - 1×10^{-2} M. [8] In another study, Tripathy *et al.*, (2017) have detected dengue virus through nanofibres of Electrospun semi-conducting Manganese (III) Oxide (Mn₂O₃) based Electrochemical DNA nanobiosensor. The limit of detection was reported to be 120×10^{-21} M [9]. Yoo *et al.*, (2017) developed a single-walled carbon nanotubes (SWCNTs)-based electrochemical nanobiosensor to detect microorganisms found in Asian dust events which is *Bacillus subtilis*. SWCNTs revealed a reliable and sensitive detection with a detection limit of 102 CFU/ml and a linear range of 102-1010 CFU/ml within 10 min of detection time [10]. Brince Paul *et al.*, (2016) designed Mercaptopropylphosphonic acid functionalized copper doped zinc oxide nanofibers and synthesized these nanofibers through electrospinning technique to detect *Plasmodium falciparum* histidine-rich protein-2. The biosensing showed detection limit of 6 attogram/ml, and detection range of 10 ag/ml-10 µg/ml with excellent sensitivity 28.5 KΩ/(gm/ml)/cm² [11] Electrochemical nanobiosensors are also widely utilized for the detection of cancer [16].

Amperometric methods

Amperometric nanobiosensors have the ability to measure the current which is produced for determining the quantity of an analyte with fixed potential and measure the current through electrochemical oxidation or reduction at the working electrode. Recently the use of this biosensors is becoming more common [17]. In this study, Mobed *et al.* developed a novel paper-based bioassay for monitoring *L. pneumophila*. Silver graphene quantum dots (Ag/GQDs) the ink was utilized for bioassay of *L. pneumophila*. The quantification and detection limit of this platform was 1ZM and linear range of cDNA was 1µM to 1ZM via using chronoamperometry technique and results revealed that despite a simple structure *L. pneumophila* has high sensitivity and specificity for the DNA based bioassay [12].

Voltammetric methods

Voltammetric nanobiosensors are most commonly used and available methods for ultrasensitive detection of various pathogens

because of their high sensitivity, the ability of simultaneous quantification of targets, selectivity and cost-effectiveness. These nanobiosensors includes different methods such as linear sweep voltammetry (LSV), square wave voltammetry (SWV), differential pulse voltammetry (DPV) and cyclic voltammetry (CV). Nguyen *et al.*, (2009) and colleagues have developed an electrochemical nanobiosensor based on membrane for sensing of inactivated West Nile viral particle and West Nile virus protein domain III (WNV-DIII) by utilizing anti-WNV-DIII immunoglobulin M (IgM) as the biorecognition probe. The detection limit of this platform was 4 pg ml⁻¹ via using voltammetric detection method and high sensitivity was achieved [13].

Membrane-based sensors

Nanobiosensors based on membrane sensors is utilized worldwide in several biomedical applications. Because of the nature of nanopores, these are used as filters for the isolation of DNA, cells, RNA, bacteria, viruses and proteins detection. They have regular and uniform spaced nanochannels, which act as templates for the incorporation of nanosized materials ranging from metals, semiconductors, polymers, metals, and biomolecules which impart the novel biological and physicochemical characteristics to enhance the applications of membrane-based sensors. Membrane-based nanobiosensors have uniform size nanopores, high surface area, cost-effective, high aspect ratio and are easy to prepare [18]. Rai *et al.*, (2012) designed ultrasensitive nanoporous membrane-based DNA biosensors using 5' aminated DNA probes and immobilized it on the alumina channel walls to detect the dengue virus (DENV). The detection limit of detection of this nanobiosensor was 9.55×10^{-12} M with a linear range of over 6 order of magnitude i.e., 10⁻¹² to 10⁻⁶ M and high specificity [14].

Overview of optical nanobiosensors

Optical nanobiosensors are used widely due to its varied advantages over conventional techniques, which include high sensitivity, specificity, small size and less cost. Optical nanobiosensors are utilized in several fields, mainly healthcare, biotechnology, environment industry. Recently, the monitoring and diagnosis of varied diseases have undergone risky variations via optical biosensors. Fluorescence nanobiosensors are one of the most common optical methods used for detection of several pathogens/viruses because of their label-free detection capability, specificity, sensitivity, and cost-effectiveness [19]. Table 2 gives a glimpse of detection values, linearity range, nanomaterials used and detection method by optical nanobiosensors for diagnosis of diseases.

Table 2: Overview of optical nanobiosensors in viral diseases

Detection method	Nanomaterial	Limit of detection	Linear range	References
Fluorescence	CdTe QDs	0.13 µg ml ⁻¹	-	[20]
Fluorescence	Oligonucleotide probes labeled with quantum dots and (AuNPs-Rh)	3×10^{-8} M	-	[21]
Fluorescence	CdTe QDs	0.2 nM	1.0 to 50.0 nM	[22]
Fluorescence	Nanobeads	10^2 - 10^3 CFU/ml	0-0.2 µM	[23]
SPRI	AuNPs induced with QDs	0.03 pg/ml and 0.4 pg/ml, 10 PFU/ml	-	[24]
Fluorescence	SiO ₂ -encapsulated alloyed CdZnSeS QDs	8.2 copies/ml and 9.3 copies/ml	-	[25]
Fluorescence	FAIA	220 pg/ml	400 pg/ml to 25 ng/ml	[26]
Microfluidic device	SERS	0.01 IU/ml	0.0125-60 IU/ml	[27]
Microfluidic chip	RT-LAMP	1 copy/µl	-	[28]

AuNPs-Rh-rhodamine-immobilized gold nanoparticles, CdTe QDs-Cadmium-telluride quantum dots, CFU-colony forming unit, AuNPs-gold nanoparticles, FAIA-fluorescent anisotropic immunoassay, SERS-surface-enhanced Raman scattering, IU= international unit, RT-LAMP-reverse-transcription loop-mediated isothermal amplification.

Gold nanoparticles

Over the past few decades, Gold nanoparticles (AuNPs) have been the subject of interest for research in biomedicine. AuNPs is also known as colloidal gold have novel diagnostic purposes or optical properties due to which it became popular worldwide in recent years for its applications in medicine. Nowadays, these AuNPs are

utilized in the entire globe as point-of-care tests and novel testing strategies since it provides more sensitive, simpler, faster and cost-effective assays to clinical laboratories [29]. In a study by Razmi *et al.*, (2019) *Tomato yellow leaf curl virus* (TYLCV) genome in plants which are infected was detected using unmodified AuNPs and eliminated the need for detection equipment/PCR amplification [30]. Wang *et al.*, (2017) utilized simple colorimetric detection

method; for this he developed unmodified gold nanoparticles as colorimetric probes and detected *Cucumber green mottle mosaic virus* (CGMMV), which is transmitted by infected cucumber seeds, leaves and soil [31]. Shawky *et al.*, (2010) also utilized colorimetric assay by developing unmodified AuNPs for direct detection of unamplified Hepatitis C virus (HCV) RNA, this assay was capable of detecting 50 HCV copies/reaction [32]. Baetsen-Young *et al.*, (2018) developed a novel unamplified genomic DNA (gDNA) nanosensor with the help of dextrin capped AuNPs to detect the causal agent of cucurbit downy mildew which is the unamplified DNA sequence from *Pseudoperonospora cubensis*, 2.94 fM of pathogen DNA was detected [33]. Kaushal *et al.*, (2019) designed the nanobiosensor based on gold nanorods (AuNRs) for the detection of foodborne bacteria due to its good electro-optical properties [34].

Fluorescence

Fluorescent nanomaterials are one of the promising approaches in optical nanobiosensors. These biosensors are also widely used as an alternative for conventional methods. In a recent study, Shokri *et al.*, 2020 has detected *citrus Tristeza virus* by fluorescence anisotropic immunoassay through targeting the virus protein, CP25 to emit copper nanoclusters. The detection limit with assay was reported as 220 pg/ml within a linear range of 400 pg/ml to 25 ng/ml [26]. Similarly, Shojaei *et al.*, (2016) reported a nanobiosensor based on fluorescence resonance-energy transfer (FRET) with the help of cadmium-telluride (CdTe) quantum dots (QDs) conjugated by a specific antibody against coat protein (CP) of CTV, and the CP were immobilized on the surface of gold nanoparticles (AuNPs) for determination of *citrus Tristeza virus* (CTV). The sensitive biosensor showed a detection limit of 0.13 µg ml⁻¹ and 93%,94 % of sensitivity, specificity respectively over enzyme-linked immunosorbent assay (ELISA) [20]. Sabzehparvar *et al.*, (2019) developed FRET-based technique nano biosensor for detecting VP2 gene of infectious bursal disease virus utilizing two oligonucleotide probes labelled with quantum dots and rhodamine-immobilized gold nanoparticles (AuNPs-Rh) and the LOD value was estimated to be 3x10⁻⁸ M [21]. Shamsipur *et al.*, (2017) also developed a nanobiosensor based on FRET by utilizing CdTe QDs, which is water-soluble and detected Human Papillomavirus 18 (HPV18). Results showed the detection limit of 0.2 nM with an increase in DNA target concentration within the linearity range from 1.0 to 50.0 nM [22]. In a study by Xu *et al.*, (2017), a fluorescence nanobiosensor was designed by combining it with nanobead-based immunomagnetic separation for detection of bacterial pathogens in food products viz; *E. coli*, *L. monocytogenes*, *S. Typhimurium*. The detection limit for these bacterial pathogens was found to be 102, 103, 103 CFU/ml in lettuce, ground beef and shrimp, respectively [23]. Adegoke *et al.*, (2016) designed an ultrasensitive QD fluorophore and exploited it as fluorescence signal generator. Further, modified silanization method for encapsulation of the thiol-capped QDs in a silica layer was modified and alloyed thioglycolic (TGA)-capped CdZnSe QDs with high photoluminescence (PL) quantum yield (QY) value of 92% were synthesized to detect the norovirus. The authors reported a detection limit of 8.2 copies/ml and 9.3 copies/ml in human serum and buffered respectively. Also, sensitivity was increased to 3-fold in comparison to norovirus RNA using TGA-capped CdZnSe QD-MBs [25].

SPR/SPRi

AuNPs show a specialized phenomenon which is commonly called as Localized Surface Plasmon Resonance (LSPR) is responsible for intense red colour. SPR has a wide range of applications for diagnostic purposes; these nanobiosensors have become popular for its measurements in molecular interactions. An SPR biosensor was fabricated by Ming-Ju Chen, Kreuter *et al.*, (1996) for the detection of insect pathogen-the baculovirus commonly called as *Autographa californica* multiple nuclear polyhedrosis virus (AcMNPV). Also, in another study, Boltovets *et al.*, (2004) detected tobacco mosaic virus (TMV) through SPR technique [35, 36]. In another study, Takemura *et al.*, (2017) developed a localized surface plasmon resonance induced immunofluorescence (SPRi) nano biosensor for detection of influenza virus H1N1 and H3N2. This biosensor was based on a gold nanoparticle-induced with quantum dot fluorescence signal. The LOD for H1N1 influenza virus was found to be 0.03 pg/ml and 0.4

pg/ml in deionized water and human serum respectively, this showed high sensitivity. Whereas, H3N2 influenza virus which was clinically isolated reported the LOD value of 10 PFU/ml [24].

Waveguide mode biosensors

Waveguide biosensors are similar to the working procedure of surface plasmon resonance biosensing. The only difference in these both is the way of conducting measurements, these biosensors conduct measurements through waveguide mode. Maldonado *et al.*, (2016) designed a bimodal waveguide (BiMW) based-photonics interferometer biosensor to detect *Escherichia coli* and *Bacillus cereus* infections caused in cirrhotic patients [37].

Microfluidic devices

Microfluidic devices are the new type of diagnostic methods which are sensitive, accurate, easy to use, and give rapid responses for dangerous viruses, including HBV, ZIKV, HIV and also in foodborne viruses. Microfluidic platforms depend upon the steps of miniaturization ranging from the preparation of the specimen to, bioreaction and further, it is detected into a unique system. The conventional techniques require much more time for the identification or detection of viruses, whereas these microfluidic devices consume less time for diagnosis and clinical treatment, which is vital for the patient's survival. Owing to the nature of these microfluidic kits, these might be advantageous in the localities with poor health facilities [38, 39]. Huang *et al.*, (2017) designed a microfluidic chip insulated with air and detected varied pathogens related to pneumonia. The pathogens which were been detected are *Mycoplasma pneumoniae*, *Staphylococcus aureus*, and methicillin-resistant *S. aureus*. 99.56% coincidence rate was determined, which reveals that the correct results were reported [40]. Kamińska *et al.*, (2015) developed surface-enhanced Raman scattering (SERS) an ultrasensitive immunoassay with a new Raman reporter and unique SERS-active substrate and incorporated this in a microfluidic device to detect hepatitis B virus (HBV). The detection limit obtained was 0.01IU/ml and high specificity was obtained [27]. Kaarj *et al.*, (2018) detected Zika virus through a wax-printed paper microfluidic chip. This microfluidic chip was developed using reverse-transcription loop-mediated isothermal amplification (RT-LAMP). This platform showed the detection limit of 1 copy/µl and also proved that this technique can also be utilized for the identification of other flaviviruses, including dengue virus, chikungunya virus, also other viral pathogens that are quickly transmitted towards field-based diagnostics [28]. Dao *et al.*, (2018) designed a new nanobiosensor based on isothermal amplification, which combines microfluidic enrichment by utilizing a concanavalin which is a functionalized microchannel consisting of asymmetric herringbone groove arrays. These nanobiosensors are utilized for rapid detection of pathogens so, with the help of this nanobiosensor Dao and his coworker's detected *Salmonella enterica* serotype *Typhimurium* bacteria which causes urinary tract infections. Due to the utilization of microfluidic enrichment the sensitivity increased by 1.76 orders of magnitude [41].

Point of care testing (POCT)

POCT is the cheap and effective medical diagnostic technique which are been utilized for the detection of varied infections or diseases caused through viruses such as, hepatitis, HIV and Influenza. POCT techniques are also used by patients at their bedside, which are classified into the following two types: the benchtop or the handled devices, which include HIV detection from salivary assay and checking of glucose levels. Some of the POC testings are based upon paper techniques which were applicable for the detection of viruses. This paper-based diagnosis is easy to use, inexpensive, and disposable, which makes it well adaptable technique. Over the course of time, for the detection of colorimetric substances, paper-based sensors were replaced through different methods, including fluorometric, chromatographic, electrochemical, microfluidics etc [42]. Zhang *et al.* and his co-workers designed a simple and effective detection method for infectious disease using quantum dots nanobeads (QDNBs) as the amplified signal indicators. This proved the detection of hepatitis B surface antigen (HBsAg) proteins and also improved the sensitivity of dot-blot immunoassay detection through amplification of fluorescent signals with quantum dot

nanobeads [43]. Darbha *et al.* demonstrated that the HIV-1 viral DNA sequence can be screened by utilizing gold nanorods. The hyper-Rayleigh scattering (HRS) proved the efficient detection of HIV-1 virus DNA with an increase in intensity, sensitivity (100 picomolar) and selectivity [44]. Griffin *et al.* also utilized the HRS technique with gold nanoparticles for the detection of hepatitis C virus (HCV). The gold nanoparticles were conjugated with HCV ssRNA tagged along with rhodamine 6G. HCV ssRNA was detected and the selectivity reached a mismatch of single-base pair [45]. Chung *et al.*, designed a nanoparticle system with a dual probe which was capable of phenotyping and detecting human pathogens. An assay of nanoparticle was designed specifically based on a sandwich hybridization technique which involved two probes of oligonucleotides to target the bacterial 16S rRNAs for the detection of amplified targeted DNAs through the utilization of a miniaturized NMR device. The magneto-DNA platform was found, which allowed universal and specific detection of varied clinically relevant bacterial species, with sensitivity down to relevant bacteria. Further, they found the assay to be robust and rapid and simultaneously diagnosed a panel of 13 bacterial species in the clinical specimen within the time limit of 2 h; also, a generic platform was formed for rapid identification of phenotype pathogens due to the varied applications [46]. In another study, Lee *et al.*, and his colleagues developed a handheld diagnostic magnetic resonance (DMR) system for fast analysis using magnetic-nanoparticles as a proximity sensor for magnification of molecular interactions. It was found that DMR system is able to perform the measurements on biological samples which are unprocessed and can also be utilized for the characterization and detection of infectious agents ranging from bacteria, fungi, viruses etc. Later, they predicted that this DMR system when combined with the strategies of microfabrication it might be utilized as a portable, affordable, high-throughput POC nano diagnostics system for detection of significant infectious diseases in the future [47]. In yet another study by Liong *et al.*, magnetic-nanoprobes have been utilized to develop the strategy of magnetic barcoding for the detection of *Mycobacterium tuberculosis* (MTB). PCR-amplified mycobacterial genes were captured on microspheres sequence-specifically, labelled by magnetic nanoprobes and were detected by NMR. The components were integrated into a fluidic cartridge for streamlined chip-operation, this platform was utilized for the detection of *M. tuberculosis* and for the identification of drug-resistant strains within 2.5 h from mechanically processed sputum samples. From the measurements of MTB-positive patient specimens, the clinical utility was demonstrated and the confirmation for the assay specificity was done clinically by non-MTB bacteria. Results demonstrated that a combination of magnetic barcode assay system with portable systems might be potential for becoming a sensitive, low-price and high throughput platform for infectious diseases point of care-diagnostics [48]. Cihalova *et al.*, also utilized magnetic barcode as a point of care diagnostics for the detection of most infectious fungal pathogens viz; *Klebsiella pneumoniae*, *Staphylococcus aureus*, methicillin-resistant *Staphylococcus aureus* and bacteria using fluorescent nanoparticle quantum dots (QDs). The results concluded that the method had the capability for the detection of infectious bacteria as low as the concentrations of 102 CFU/ml [49]. In a study by Inci *et al.*, a unique nanoplasmonic-based sensor was developed for the detection of HIV at different concentrations by using immobilized antibodies for capturing rapidly evolving viral subtypes selectively. Results demonstrated that detection of data analysis took 10 min and exhibited high sensitivity, specificity and repeatability of 98±39 copies/ml. It also specified that the viral diseases detection directly from unprocessed blood samples of patients were feasible, showed a significant step towards POC tests at resource-constrained settings, hospitals etc. by enabling rapid detection, isolation, quantification and capture of viruses [50]. Kosaka *et al.* and his co-workers designed an immunoassay by the combination of both nano-mechanical properties of gold nanoparticles and opto-plasmonic transduction methods. By this immunoassay HIV-1, capsid antigen p24 in the human serum was detected. The limit of detection was reported to be 10-17 g/ml. and it was proved that this technology meets the demands to be produced *en masse* at a much lower cost, the capability for the miniaturization can be used as a point of care tests and also proved

this platform to be an easily adaptive technique for diagnosis compared to Nucleic acid amplification tests (NAAT) [51]. Islam *et al.* developed a smart nanosensor utilizing graphene-based field effective transistors and detected HIV-related diseases, including renal arthritis (RA) and cardiovascular diseases (CVDs). Graphene was functionalized with aminoalkanes and was conjugated covalently with varied antibodies such as anti-p24 for HIV, anti-cyclic citrullinated peptide (anti-CCP) for RA and anticardiac troponin 1 (anti-cTn1) for CVDs via carbodiimide activation for detection of various biomarkers. Results concluded that high sensitivity with good linear curve was exhibited, the limit of detection for various antibodies were reported to be 10fg/ml for cTn1 and CCP and 100fg/ml for p24. Further, they concluded that the nanobiosensor based on graphene confirmed excellent performance and can be utilized for the on-site detection of HIV, Rheumatoid Arthritis and Cardiovascular diseases biomarkers in real samples [52]. Ng *et al.*, proved the extensive utilization of POC system to detect HIV in saliva, leukocytosis in whole blood and plasma by utilizing mobile-based magneto-nano sensor arrays and magnetic nano-particles. This utilization of mobile-based magneto nano sensor device proved the ability to detect HIV in saliva and leukocytes in plasma quantitatively at a point of care within the assay time of 16 min with an accuracy of 90%, 80% respectively. Thus, they concluded that the portability, high sensitivity and ease of use of their nanodevice has the potential for becoming a low-cost and high throughput platform for point of care-diagnosis of HIV and early detection of diseases [53].

Nucleic acids-and protein-based nanobiosensors

Recently a newly based technique of nucleic acids-and protein-based nanobiosensors has been developed for detection of the novel emerging COVID-19 virus. The high specificity, selectivity and rapid biosensing activity of nanobiosensors have made it useful for the detection of specific proteins or nucleic acids of COVID-19.

Immunoglobulin (Ig)-based nanobiosensors

Immunoglobulin (Ig)-based nanobiosensors have also been utilized for the detection of newly emerging COVID-19 virus since our system can produce Ig in the face of COVID-19 utilizing nanobiosensor-based serological tests to determine specific antibodies which might be helpful.

Sharifi *et al.*, recently showed these two reported diagnostic methods viz; nucleic acids-and protein-based nanobiosensors and Immunoglobulin (Ig)-based nanobiosensors for the detection of COVID-19 virus [54].

Conclusion and future prospects

Nanotechnology has significantly increased its demand in the development of biosensors and, has been proved useful for the detection of pathogens/viruses. Generally, the transduction mechanisms of these nanobiosensors have improved significantly due to the utilization of various nanoparticles for immobilization of enzymes, nanomaterials and nanostructures like those of quantum dots and hybrid nanostructures with varied functionalities. Unique advantages of these nanobiosensors over the assays of traditional methods such as low-price and high throughput platform, high sensitivity, specificity, rapid, reliable and real-time detection have made these nanobiosensors suitable for the detection of varied viruses. The use of nanobiosensors for POC testing has also enhanced sensitivity and became an appropriate signal amplification method. Some of the nanobiosensors have reached the limit of detection value in the picomolar and femtomolar range, due to which innovative strategies in the diagnosis of early-stage viruses is been provided *in vivo* and *in vitro*. However, the nanomaterials (NMs) biosafety must be observed in the utilization of nano biosensors for *in vivo* virus detection. Additionally, further efforts are required for the development of a nanosensing platform for detection of different virus-related diseases *in vivo* because most of the nanobiosensors have been employed for *in vitro* quantification. The more advancement and remarkable progress in the nanosensing platform with potential diagnostic features are expected to occur in future.

Table 3: List of abbreviations

HIV	Human immunodeficiency virus
ZIKs	Zika virus
DNA	Deoxyribonucleic acid
RT-PCR	Reverse transcription polymerase chain reaction
ELISA	Enzyme-linked Immunosorbent assay
TLRs	Toll-like receptor proteins
DENV	Dengue virus
QDs	Quantum dots
AuNPs	Gold nanoparticles
LOD	Limit of Detection
FRET	Fluorescence resonance-energy transfer
SPR	Surface Plasmon Resonance
SPRi	Surface plasmon resonance induced immunofluorescence
SERS	Surface-enhanced Raman scattering
POCT	Point of care testing
QDNBs	Quantum dots nanobeads
HBsAg	Hepatitis B surface antigen
HRS	Hyper-Rayleigh scattering
DMR	Diagnostic magnetic resonance
NAAT	Nucleic acid amplification tests
NMs	Nanomaterials
CVDs	Cardiovascular diseases
RA	Renal Arthritis

RESPONSE TO COMMENTS

The names of all the authors along with affiliations are included carefully in the main body of the manuscript.

Punctuation errors are rectified cautiously.

FUNDING

Nil

AUTHORS CONTRIBUTIONS

All the authors have contributed equally.

CONFLICT OF INTERESTS

Declared none

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